

A photograph of a modern, multi-story building with a curved glass facade and illuminated interior spaces. The building is set against a dark sky with some clouds. In the foreground, there is a paved area with some low walls and a small tree.

Stanford

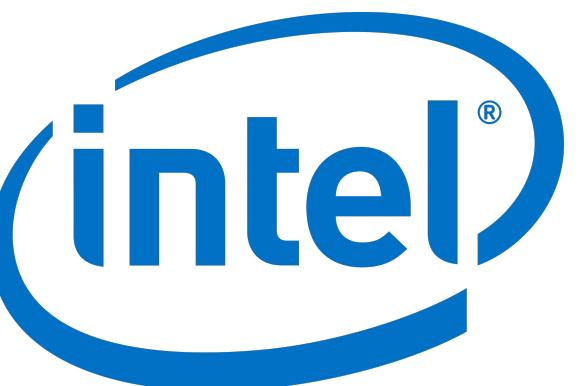
Learning Reduced-Order Models for Blood Flow Simulations using Graph Neural Networks

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Mathematical and Scientific Machine Learning
ICERM — Brown University
June 6th 2023





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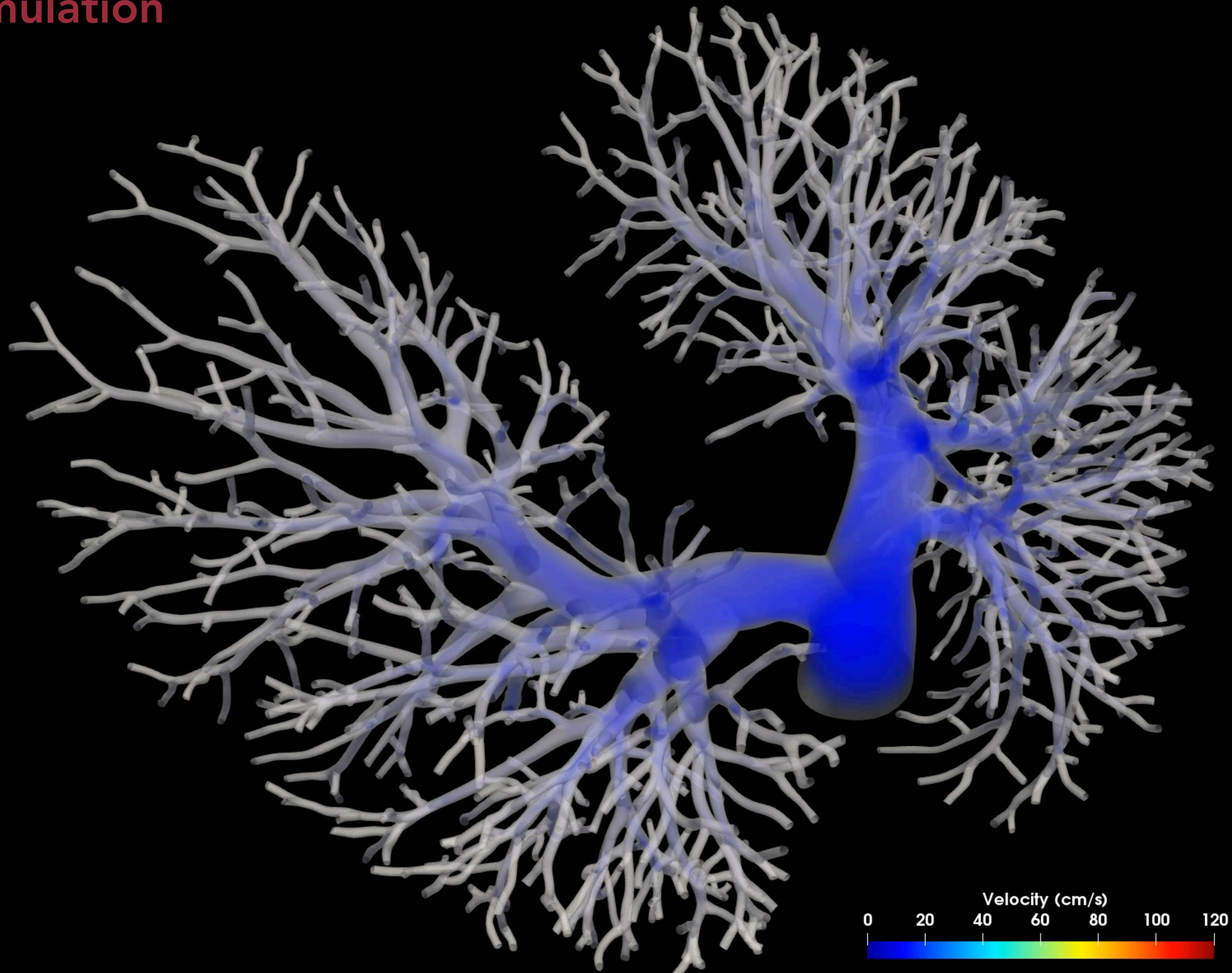


Prof. A. Marsden

Pegolotti et al. *Learning Reduced-Order Models for cardiovascular simulations with Graph Neural Networks*. arXiv <https://arxiv.org/abs/2303.07310v1> (2023)

Why simulation

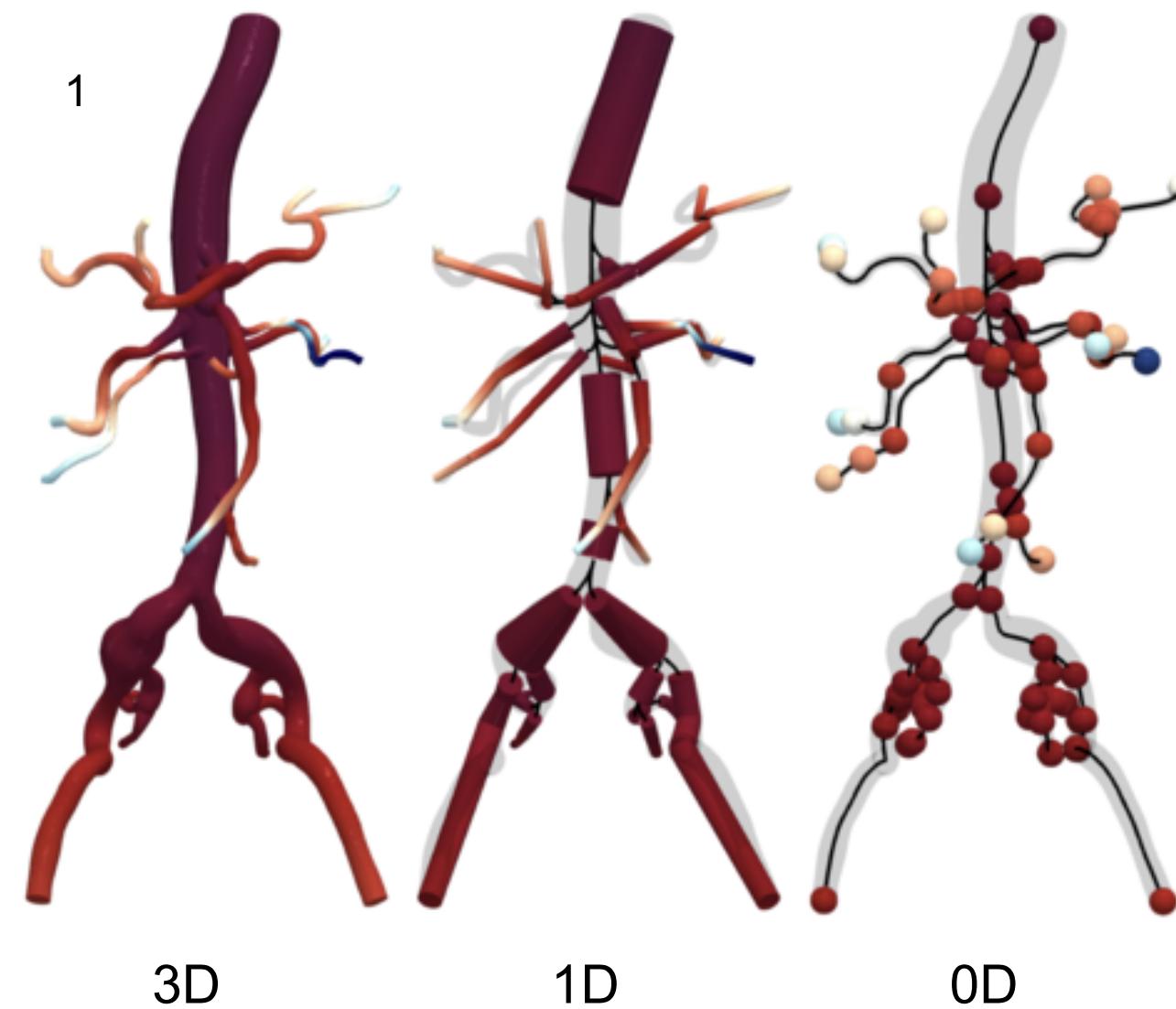
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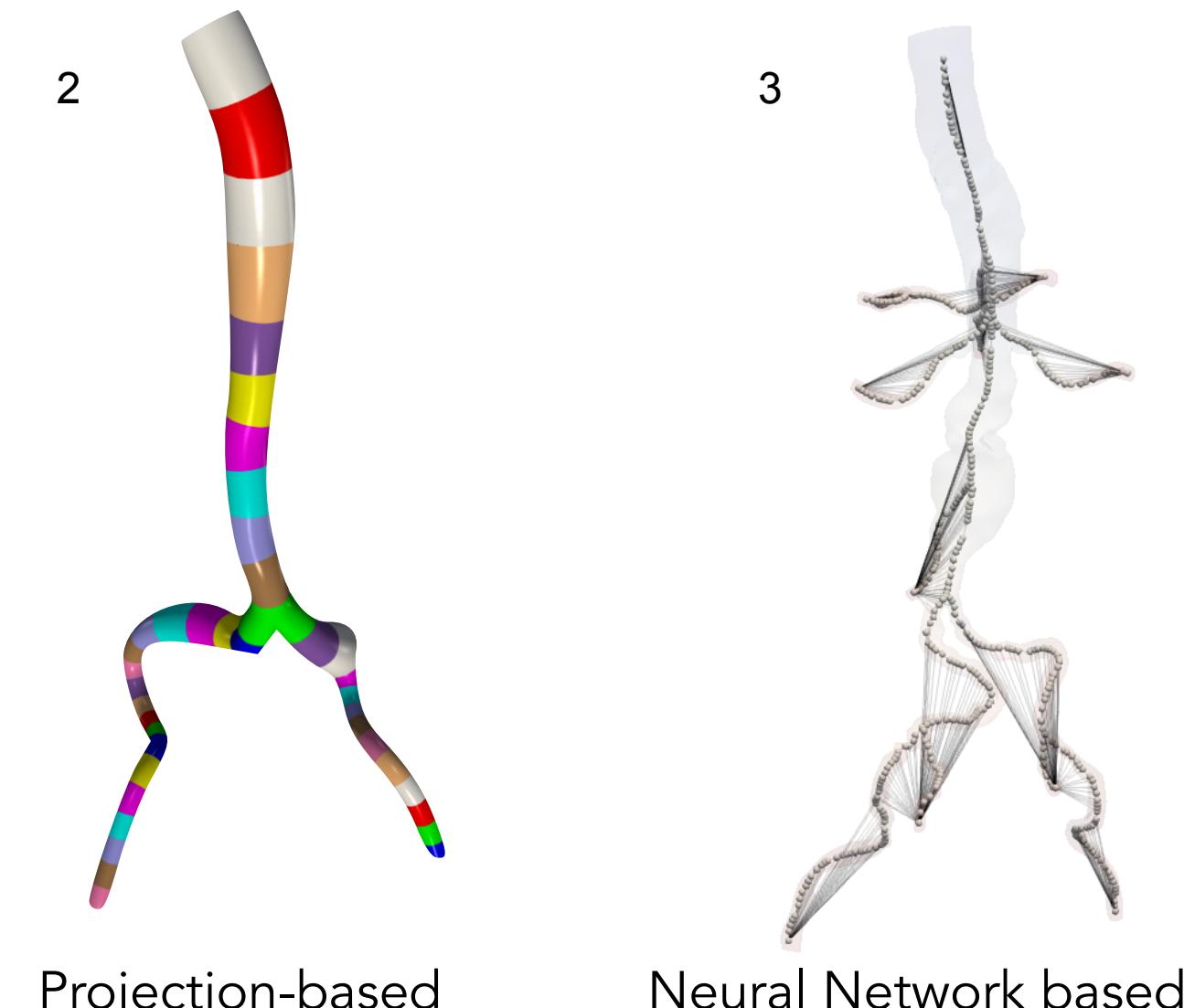
$O(10^6)$
elements
16 hours on
128 cores

Reduced-Order Models

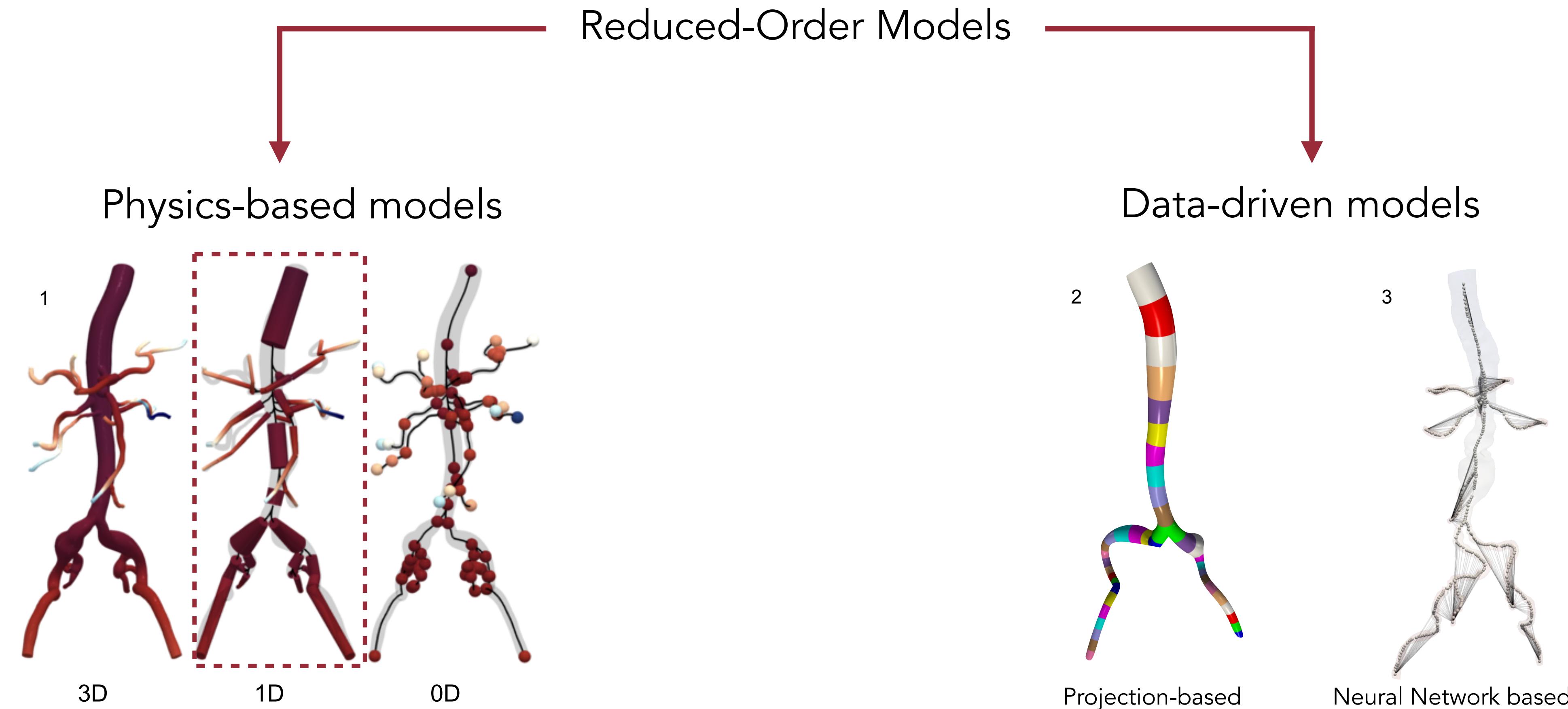
Physics-based models



Data-driven models



1. Pfaller et al. Automated generation of 0D and 1D reduced-order models of patient-specific blood flow. *Int. J. for Num. Met in Bio. Eng.* (2021)
2. Pegolotti et al. Model order reduction of flow based on a modular geometrical approximation of blood vessels. *Comp. Meth. in Appl. Mech. and Eng.* (2021)
3. Pegolotti et al. Learning Reduced-Order Models for cardiovascular simulations with Graph Neural Networks. *arXiv* <https://arxiv.org/abs/2303.07310v1> (2023)



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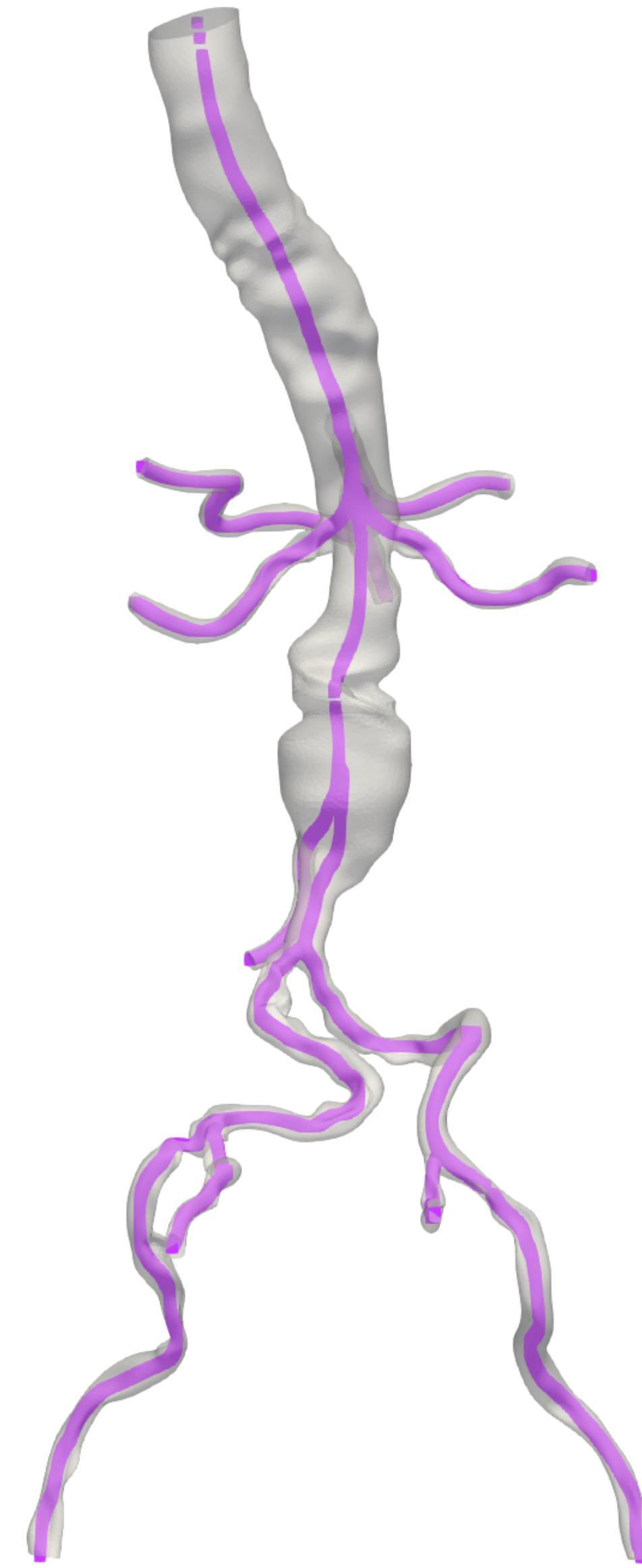
Equations:

$$\frac{\partial A}{\partial t} + \frac{\partial q}{\partial z} = 0$$

$$\frac{\partial q}{\partial t} + \frac{\partial}{\partial z} \left(\frac{4}{3} \frac{q^2}{A} \right) = -8\pi\nu \frac{q}{A} + \nu \frac{\partial^2 q}{\partial z^2} - \frac{A}{\rho} \frac{\partial p}{\partial z}$$

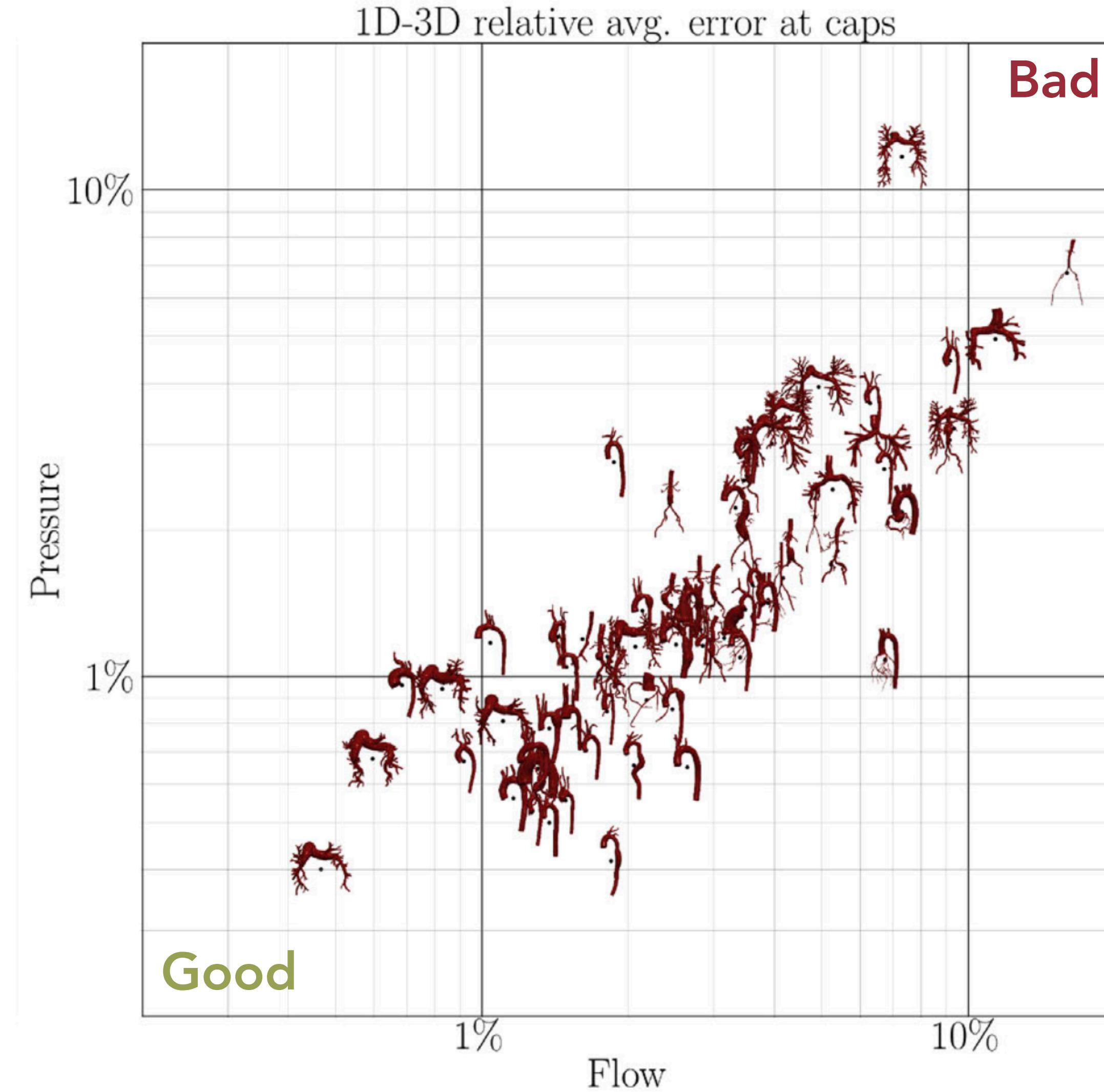
Constitutive Model:

$$p(z, t) = p_0(z) + \frac{4}{3} \left(k_1 e^{k_2 r_0(z)} + k_3 \right) \left(1 - \sqrt{\frac{A_0(z)}{A(z, t)}} \right)$$



The problem

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Pfaller et al. Automated generation of 0D and 1D reduced-order models of patient-specific blood flow. *Int. J. for Num. Met in Bio. Eng.* (2021)

Physics-based zero/one-dimensional models may be inaccurate when (i) **multiple junctions** or (ii) **severe pathological conditions** are present.

The Vascular Model Repository (VMR)

Stanford

Available at www.vascularmodel.com

The screenshot shows the homepage of the Vascular Model Repository (VMR). The header features the VMR logo and a navigation bar with links for Home, Repository, Contributors, and Contact us. The main background is a dark blue gradient with numerous 3D vascular models of various colors (red, green, blue, yellow) floating across it. In the center, the text "VASCULAR MODEL REPOSITORY" is displayed in large white capital letters, with "An open-source database of cardiovascular models" in smaller text below it. A white button labeled "Open the database" is centered on the page. Below the main banner, the word "ABOUT" is prominently displayed in large black capital letters. Underneath "ABOUT" are three sections: "What it is" (with a document icon), "Who it is for" (with a person icon), and "Our sponsors" (with a heart icon). Each section contains descriptive text and a QR code to the right.

ABOUT

What it is

A library of computational models of normal and diseased cardiovascular models.

Who it is for

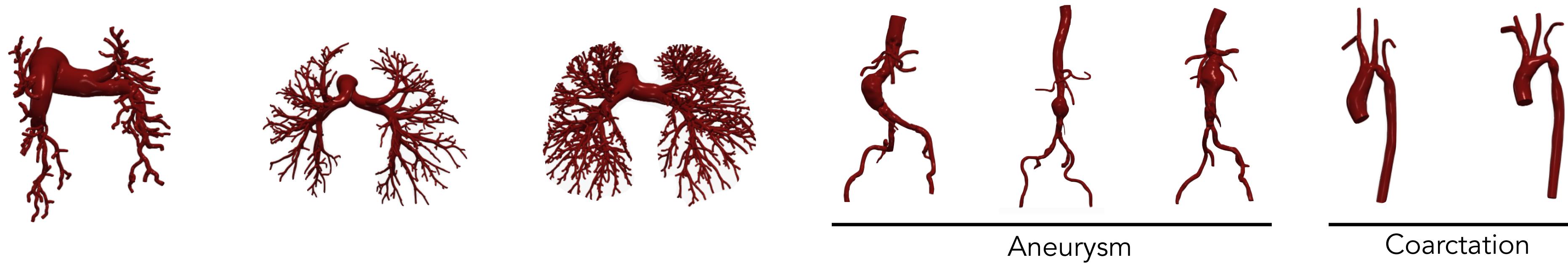
Academic, government and industry researchers. Our models can be used to verify computational methods for fluid and solid mechanics.

Our sponsors

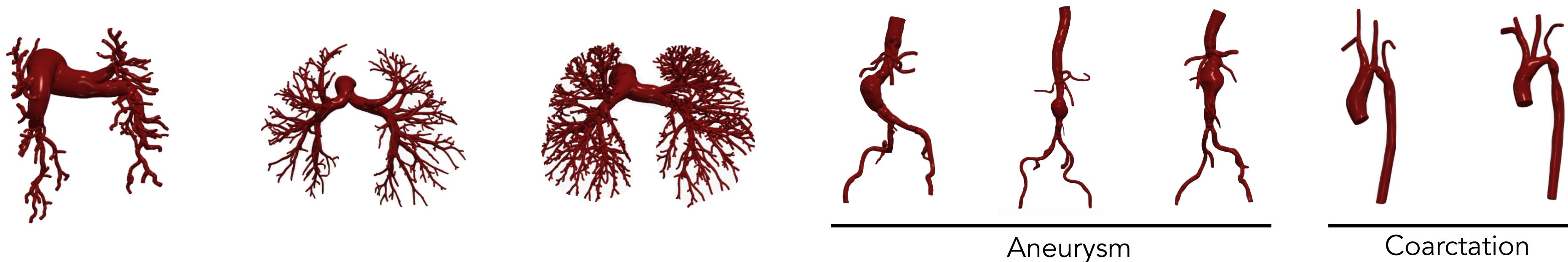
The National Institutes of Health (NIH) under the direction of the National Heart, Lung, and Blood Institute (contract HHSN268201100035C) and t



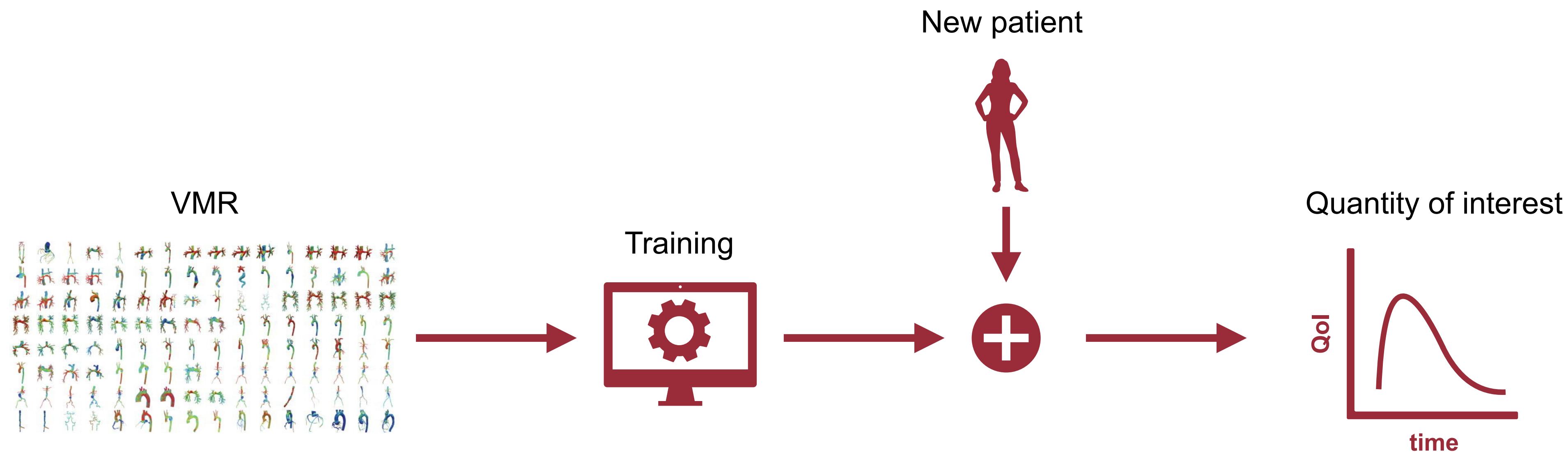
Data-driven treatment of **junctions** and **pathological conditions**

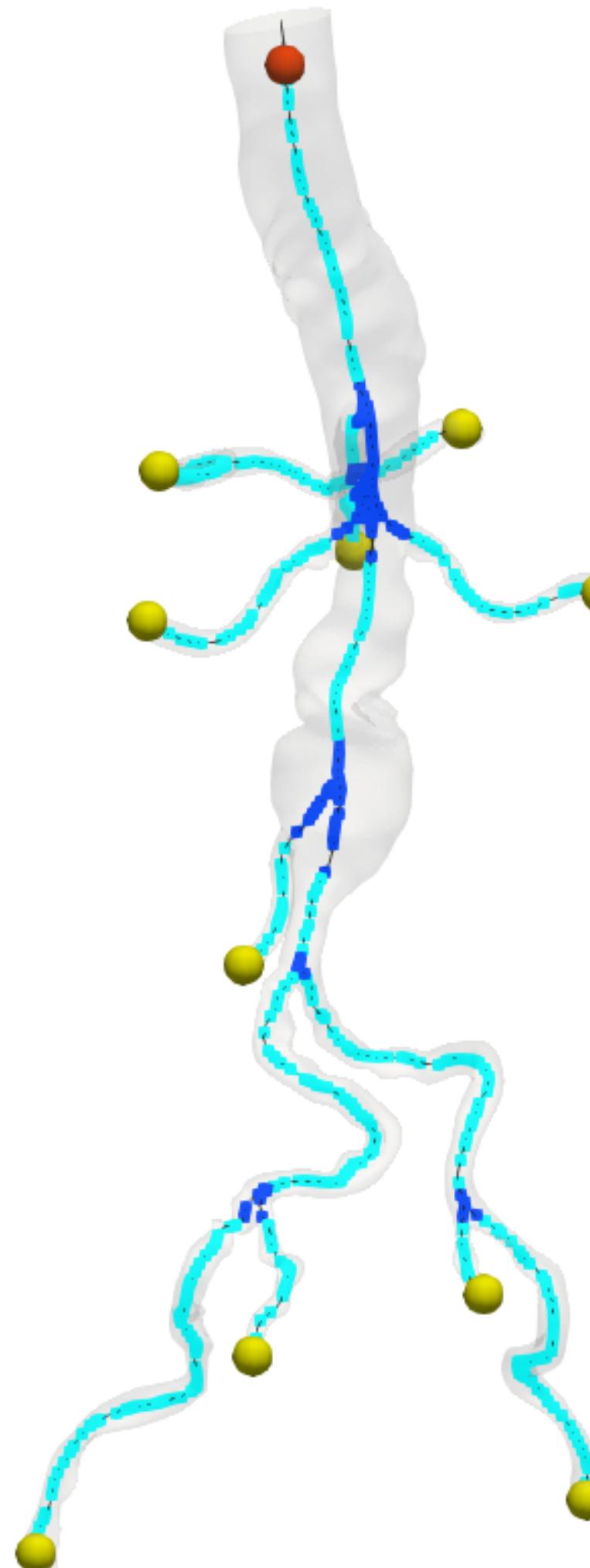


Data-driven treatment of **junctions** and **pathological conditions**



Flexibility with respect to geometry (**one trained ML model - many patients**)





Centerline nodes = graph nodes

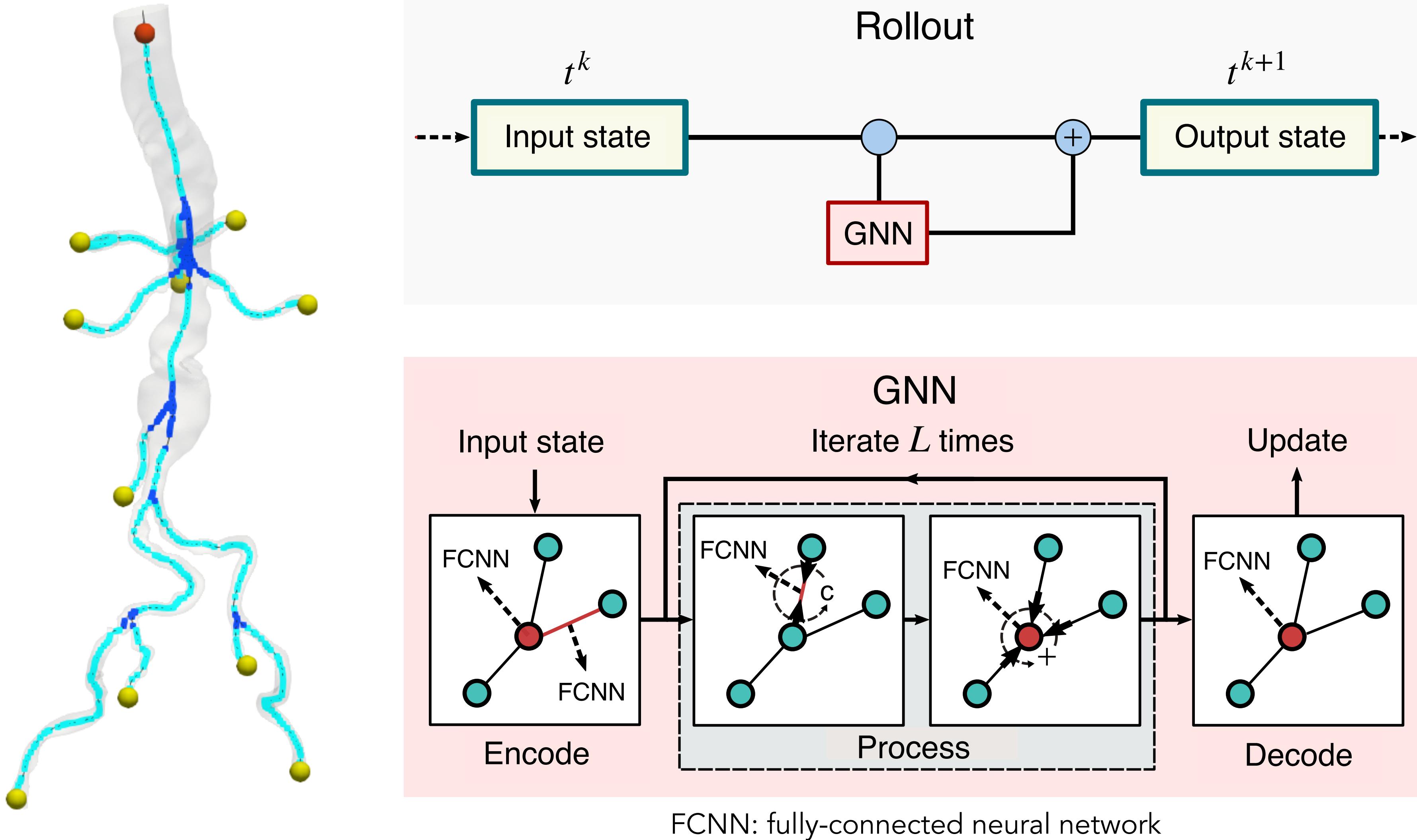
Associate features to each node and edge

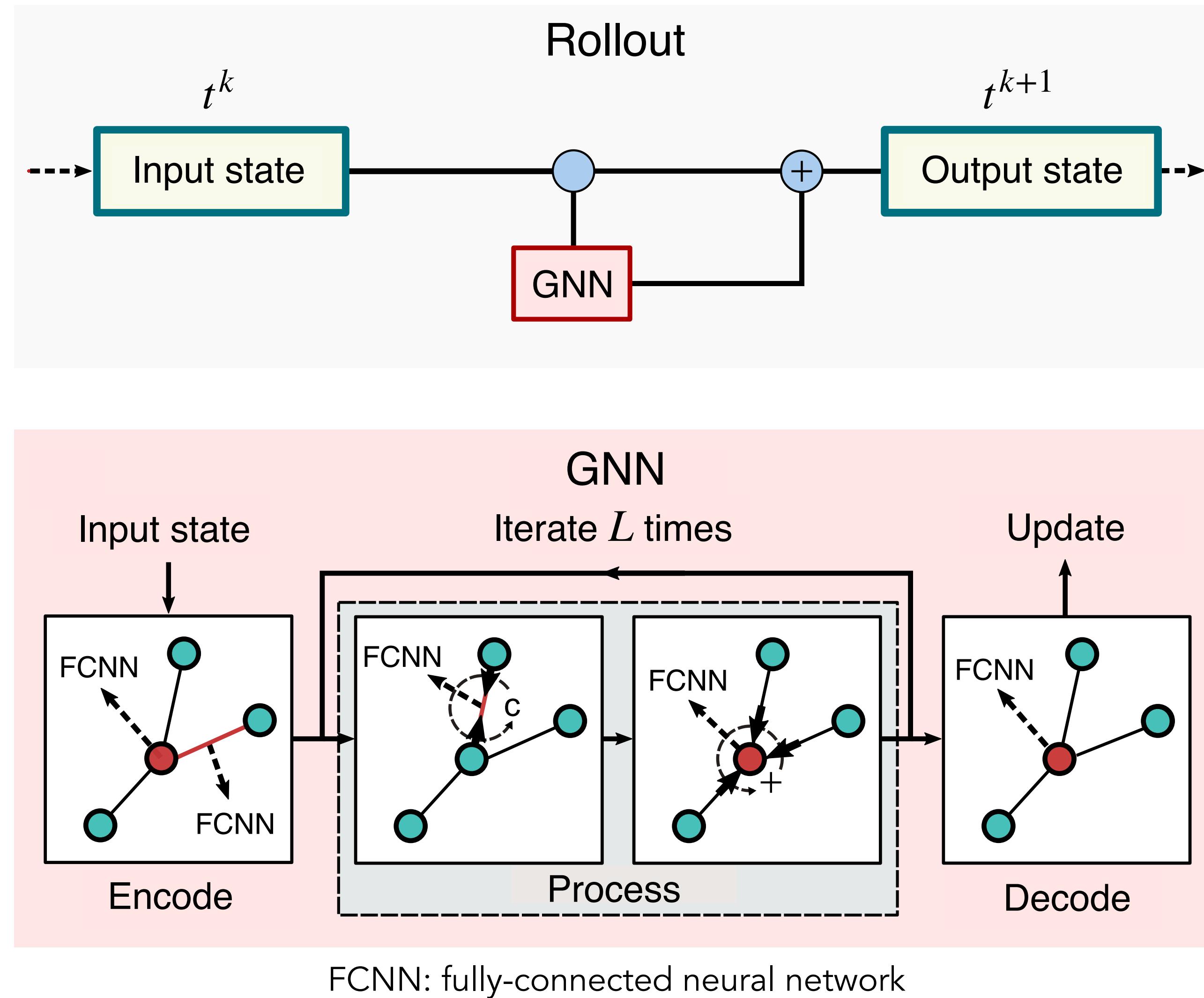
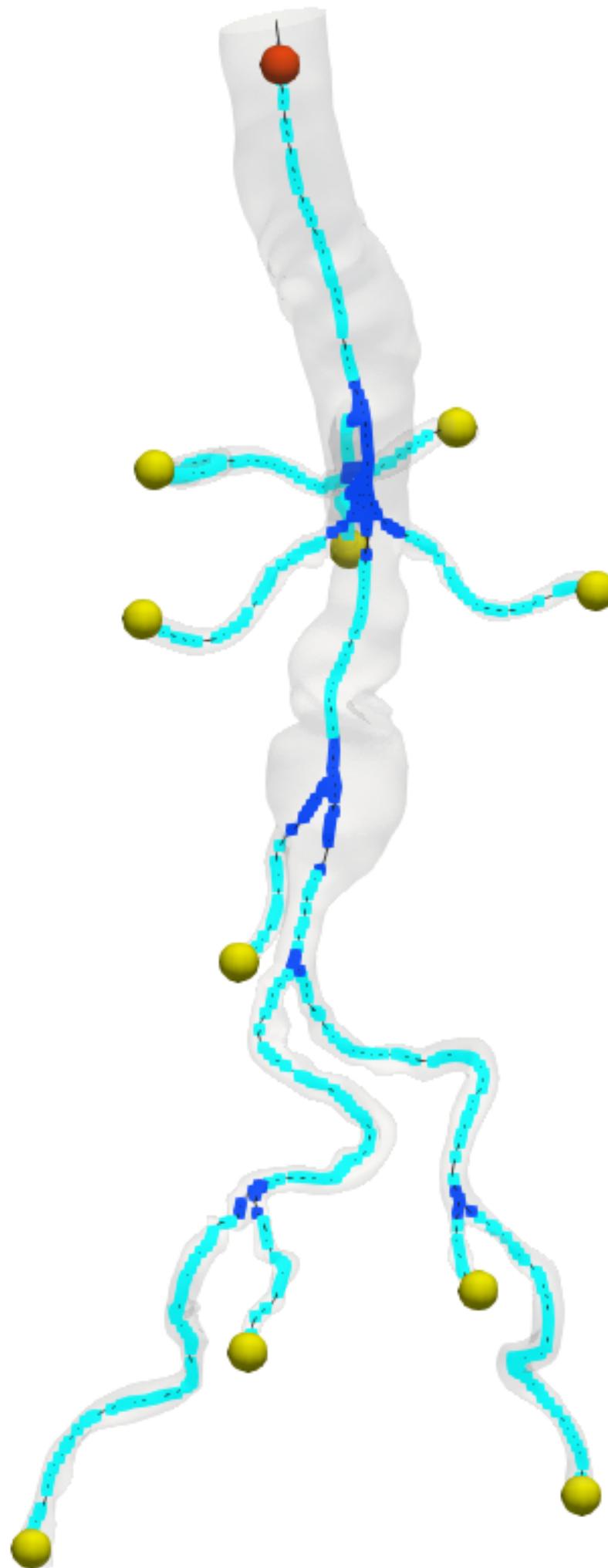
Node feature	Definition
p_i^k	Pressure at time t^k
q_i^k	Flow rate at time t^k
A_i	Cross-sectional area
α_i	Nodal type
ϕ_i	Centerline tangent
T_{cc}	Cardiac cycle duration
p_{\min}	Minimum pressure (across cardiac cycle)
p_{\max}	Maximum pressure (across cardiac cycle)
$R_{i,p}$	R_p Parameter in RCR boundary conditions
C_i	C Parameter in RCR boundary conditions
$R_{i,d}$	R_d Parameter in RCR boundary conditions
l^k	Boolean load variable at time t^k

Table 1: Node features and their definitions.

Edge feature	Definition
$\mathbf{d}_{ij}^T / \ \mathbf{d}_{ij}\ $	Normalized vector distance between node i and j
z_{ij}	Shortest path length between node i and j
β_{ij}	Edge type

Table 2: Edge features and their definitions.





Process sub-steps

1. $\mathbf{w}_{ij}^{(l)} = \mathbf{f}(\mathbf{w}_{ij}^{(l-1)}, \mathbf{v}_i^{(l-1)}, \mathbf{v}_j^{(l-1)})$
2. $\mathbf{v}_j^{(l)} = \mathbf{f}(\mathbf{v}_j^{(l-1)}, \sum_{i: \exists e_{ij}} \mathbf{w}_{ij}^{(l)})$

Main modifications w.r.t. original MeshGraphNet (1)

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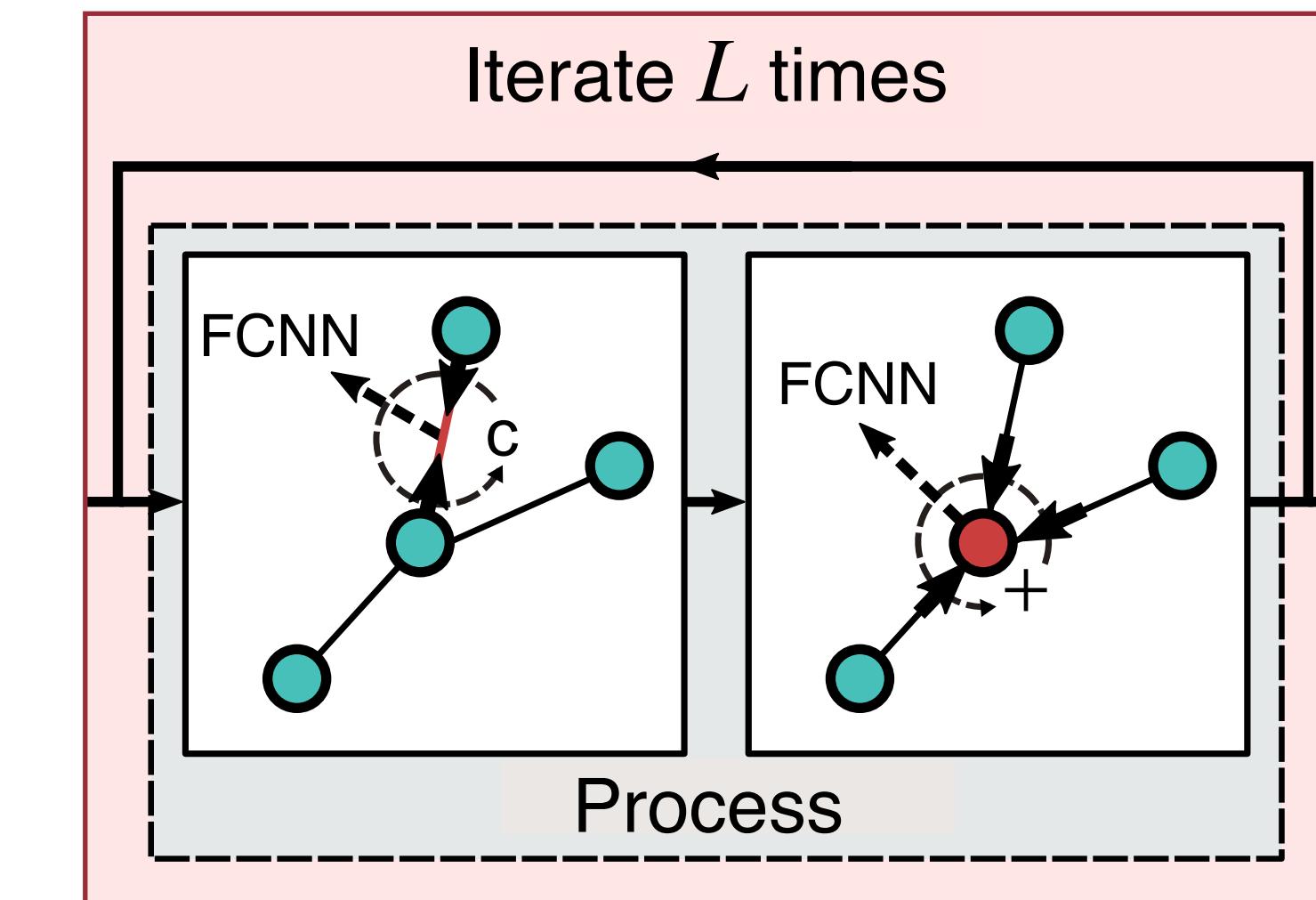
Add boundary
edges

Main modifications w.r.t. original MeshGraphNet (1)

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We want to keep
 L as small as
possible



Add boundary
edges

Main modifications w.r.t. original MeshGraphNet (2)

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Node feature	Definition
p_i^k	Pressure at time t^k
q_i^k	Flow rate at time t^k
A_i	Cross-sectional area
α_i	Nodal type
ϕ_i	Centerline tangent
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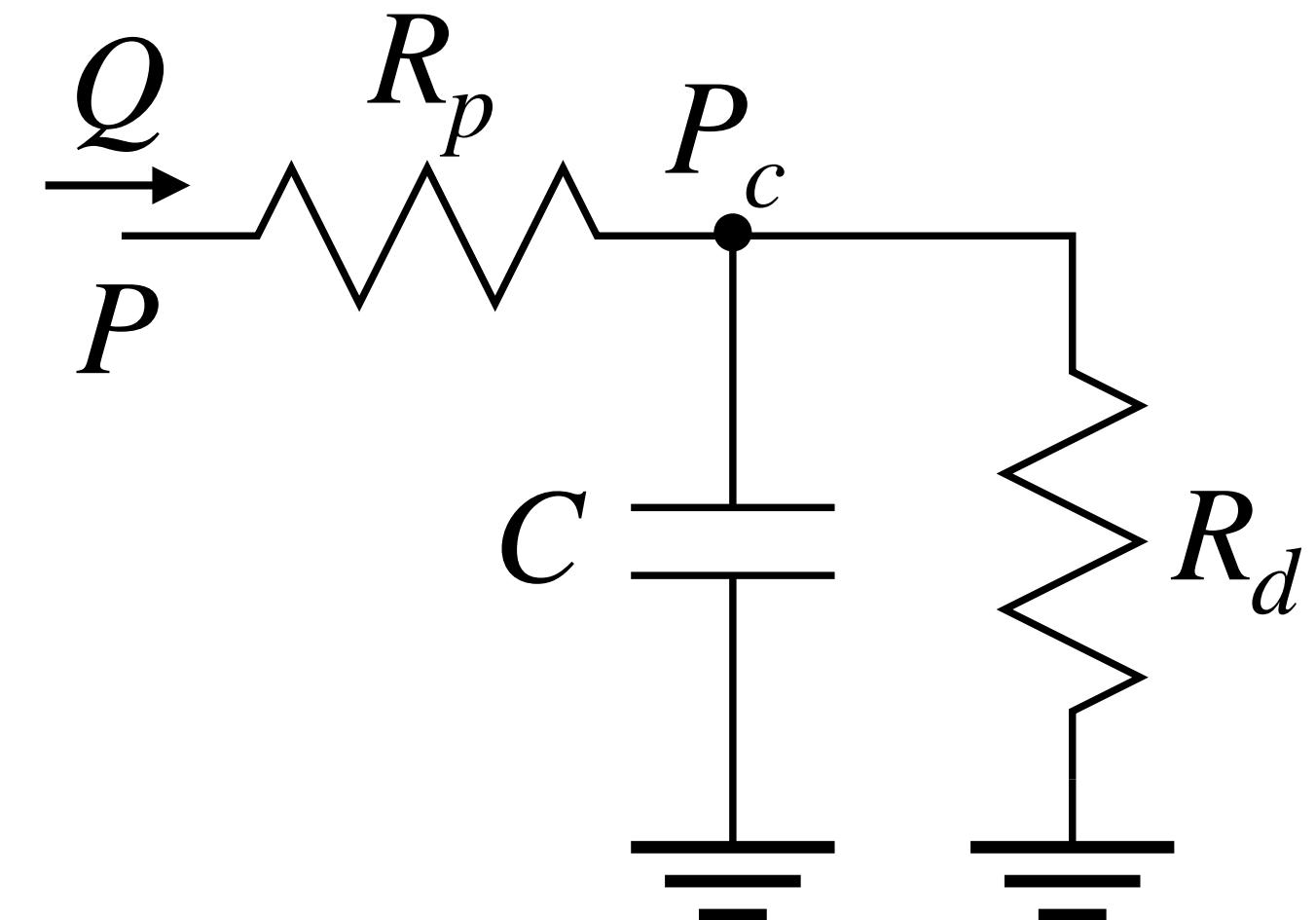
Add application-specific features (: included in the original MeshGraphNet)

Main modifications w.r.t. original MeshGraphNet (2)

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Node feature	Definition
p_i^k	Pressure at time t^k
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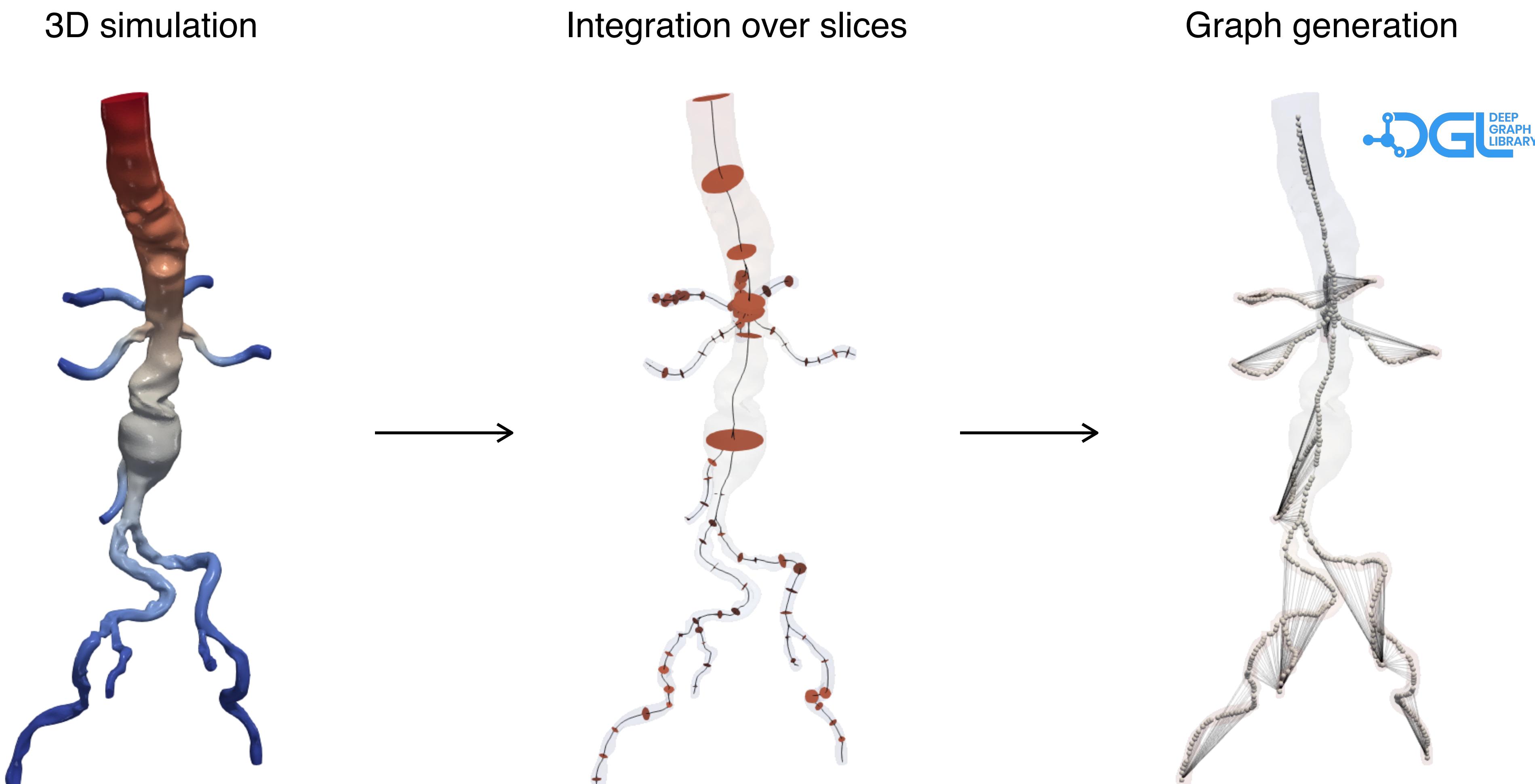
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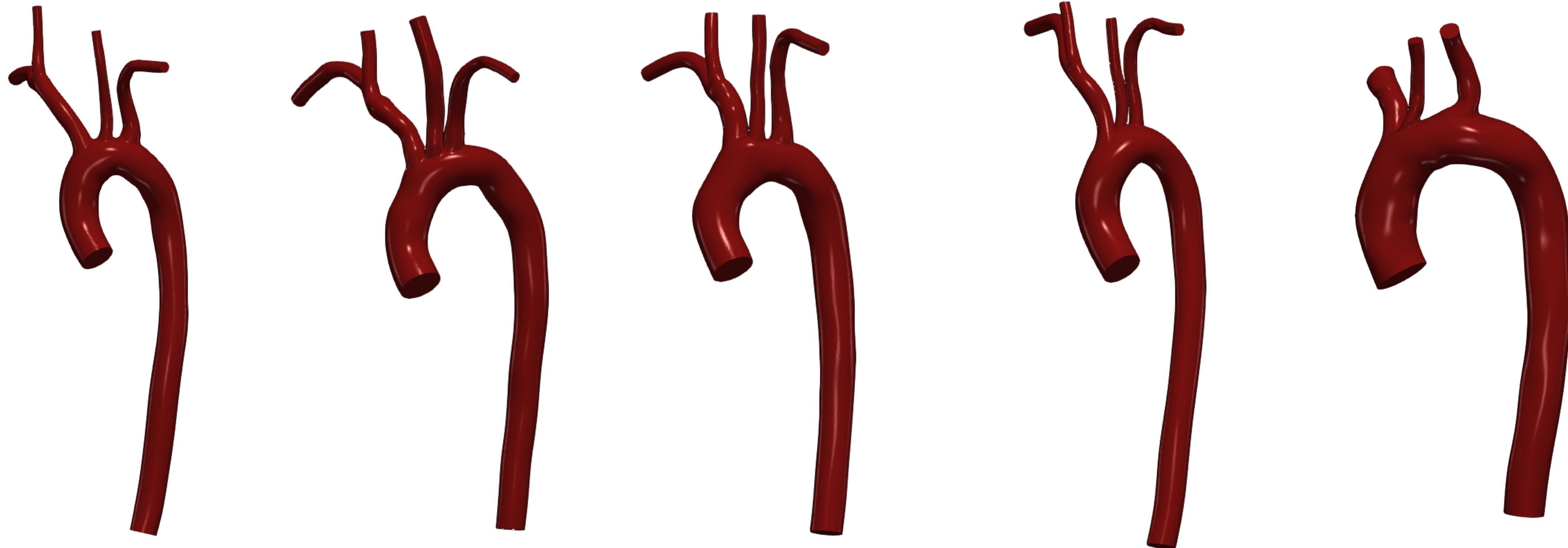
Add application-specific features (: included in the original MeshGraphNet)

Data generation pipeline

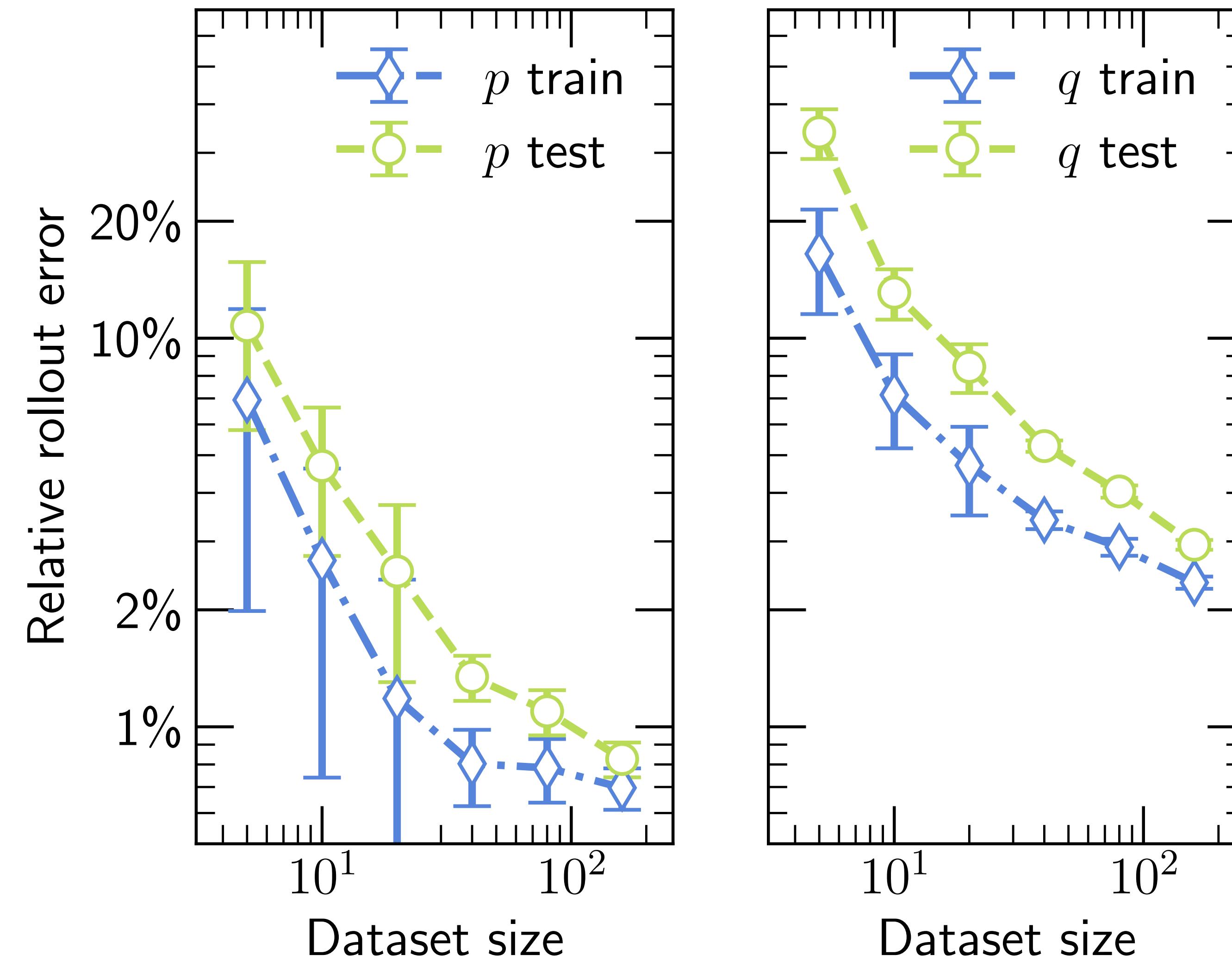
Stanford

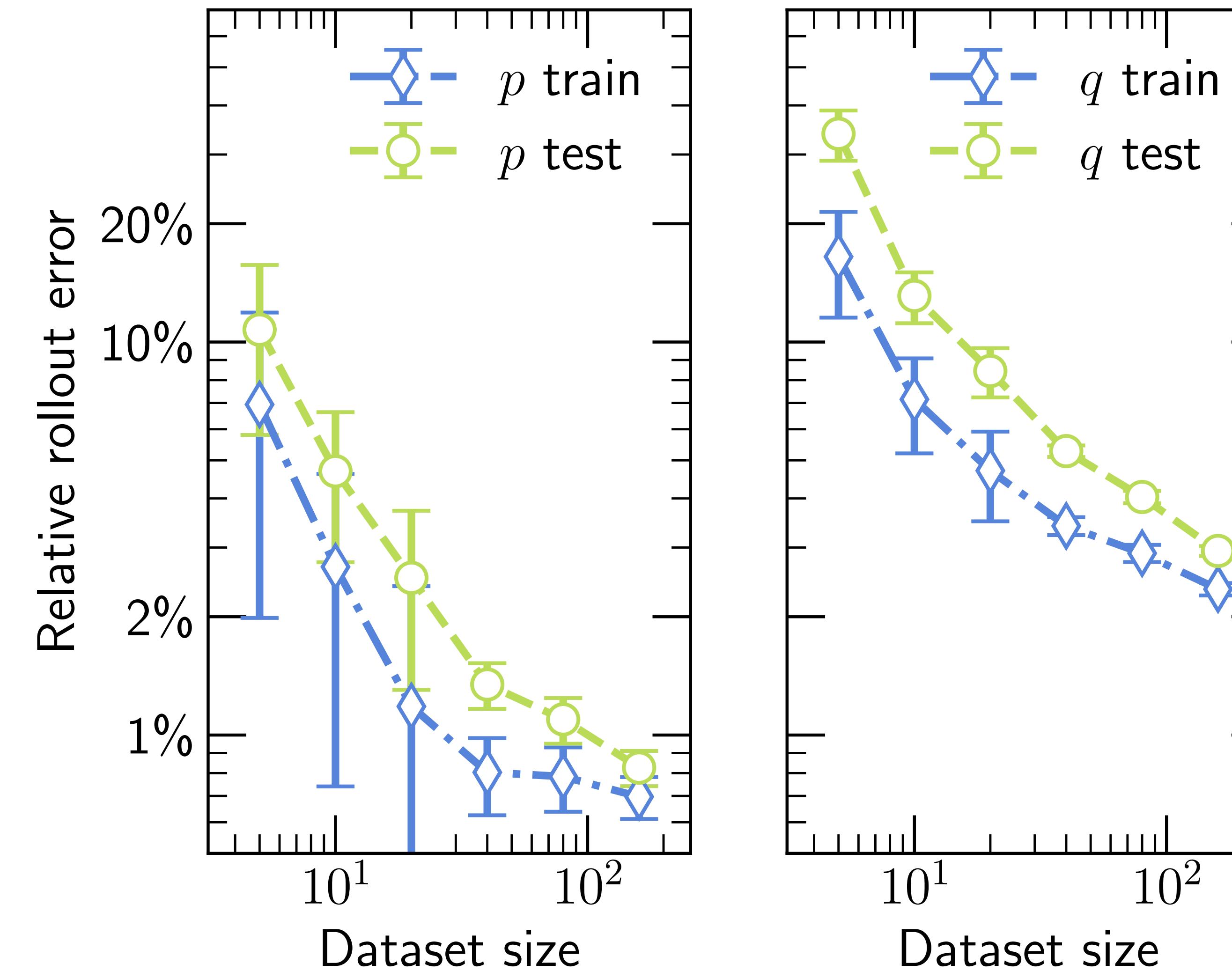


Goal: study error convergence as we consider more and more trajectories for training.

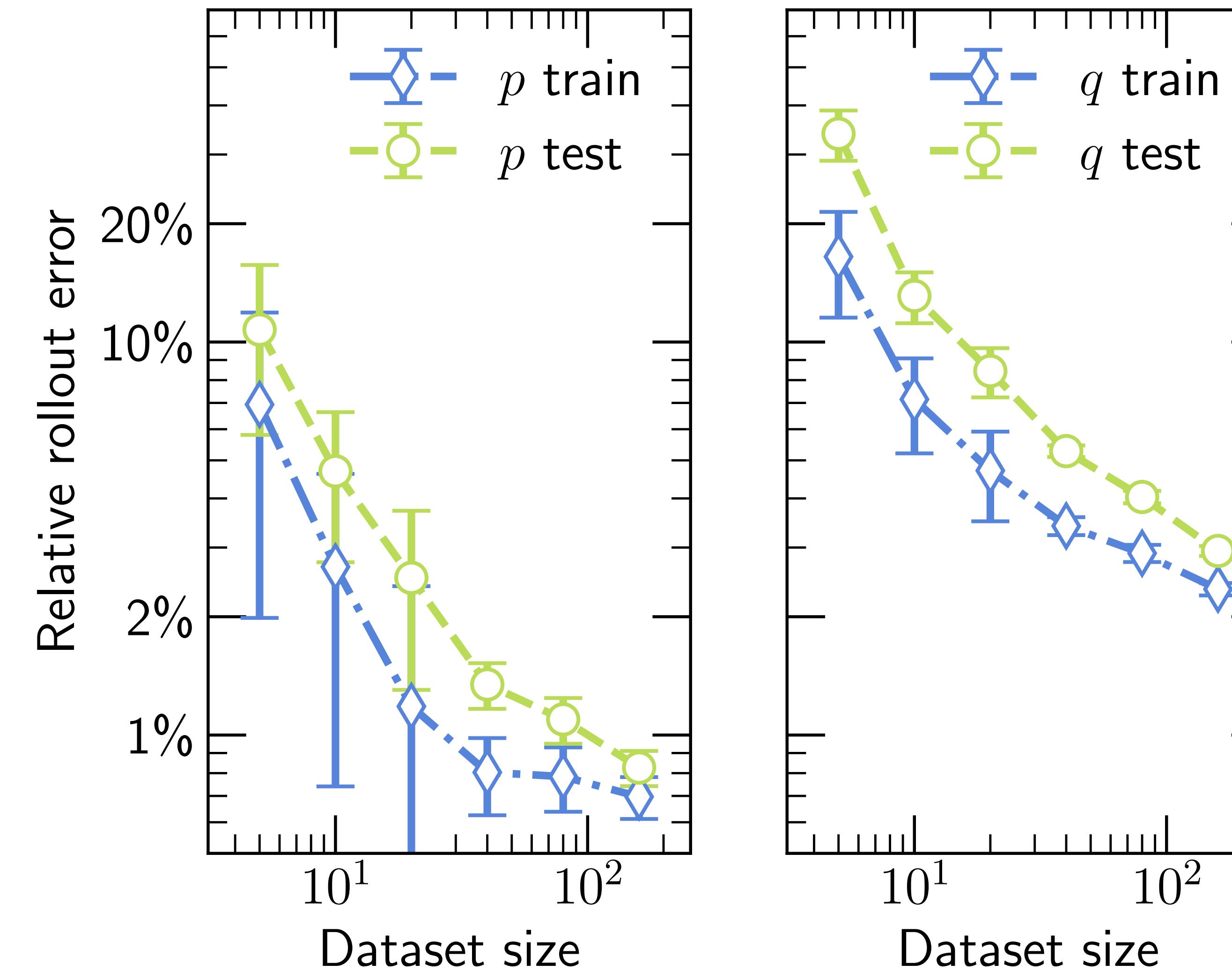


We performed 32 simulations with different boundary conditions for each of these geometries.





Error decreases as dataset size increases

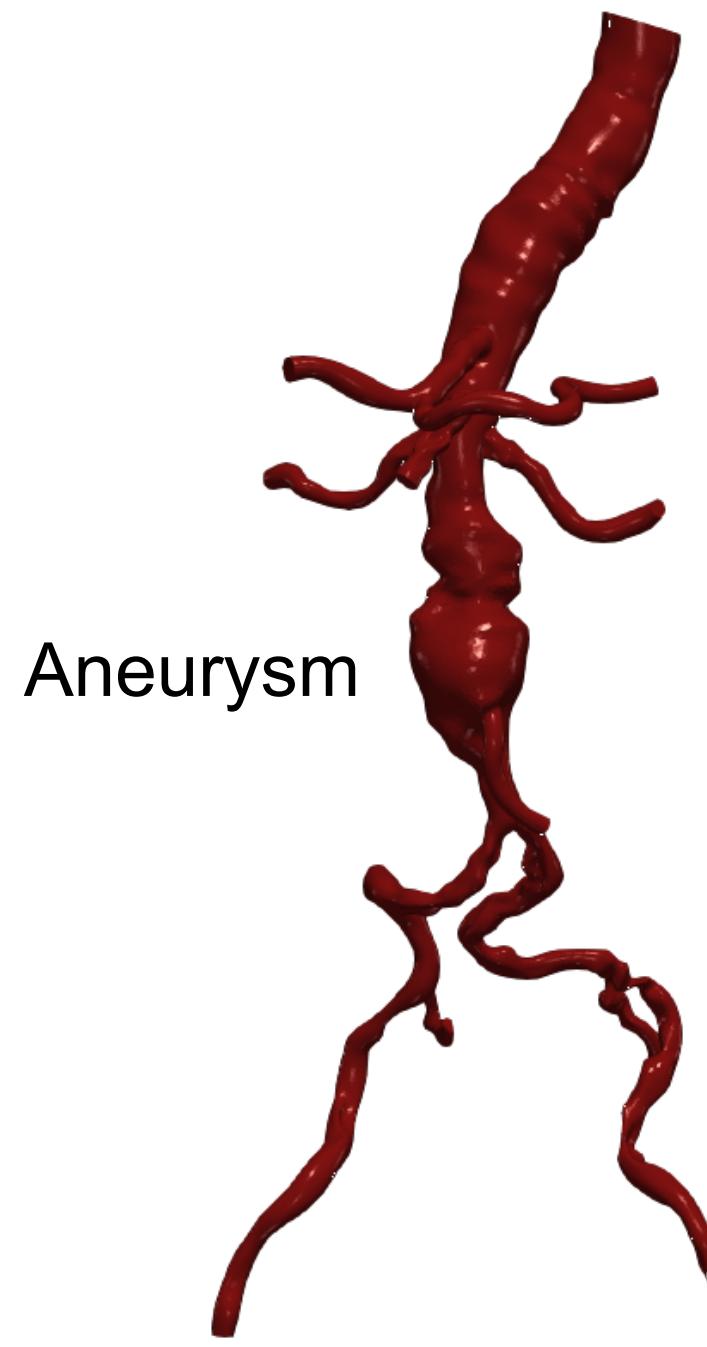


Error decreases as dataset size increases

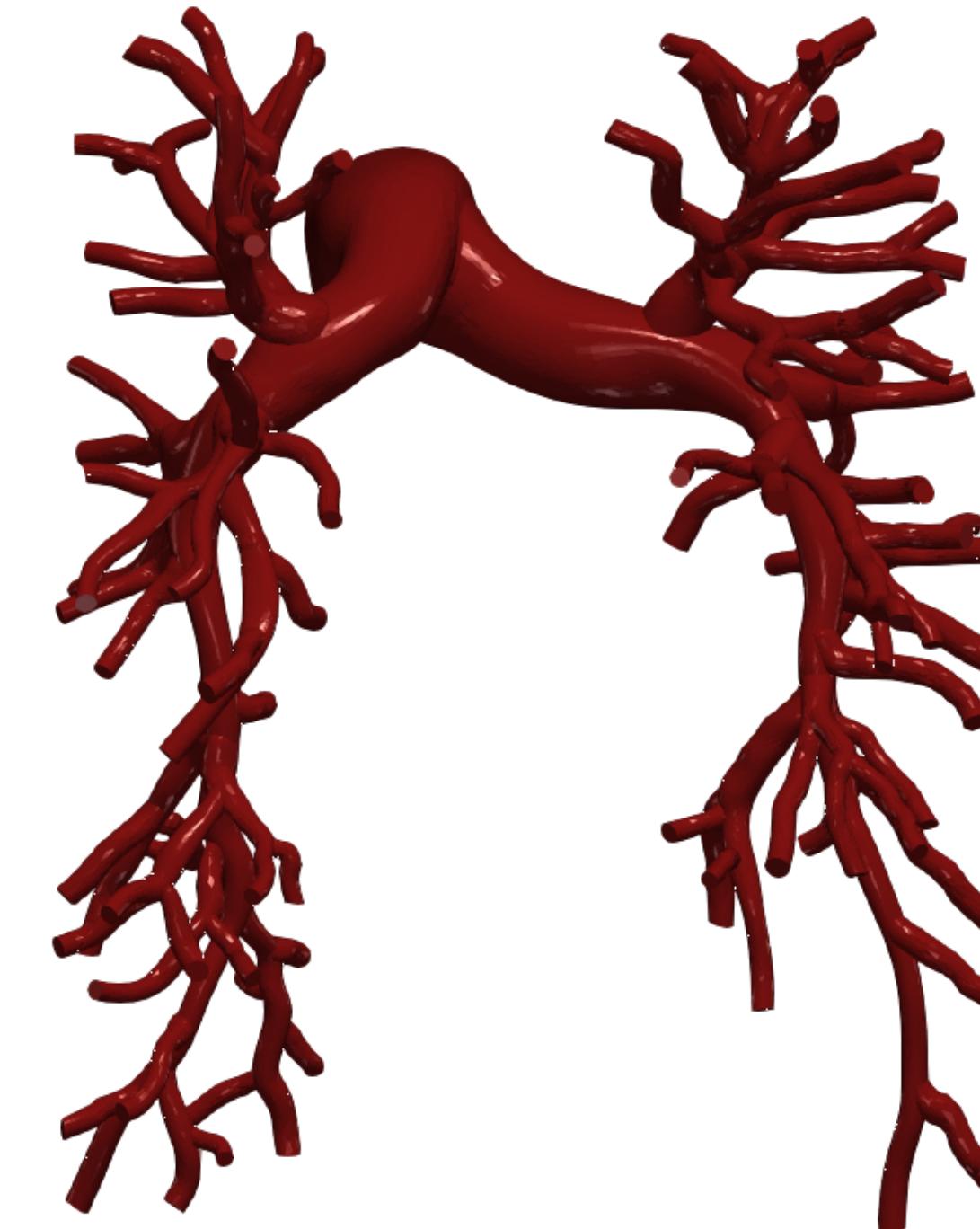
Generalization error decreases as dataset size increases

Goal 1: train a single GNN on diverse anatomies.

Goal 2: compare performance against physics-based one-dimensional models.



Aneurysm

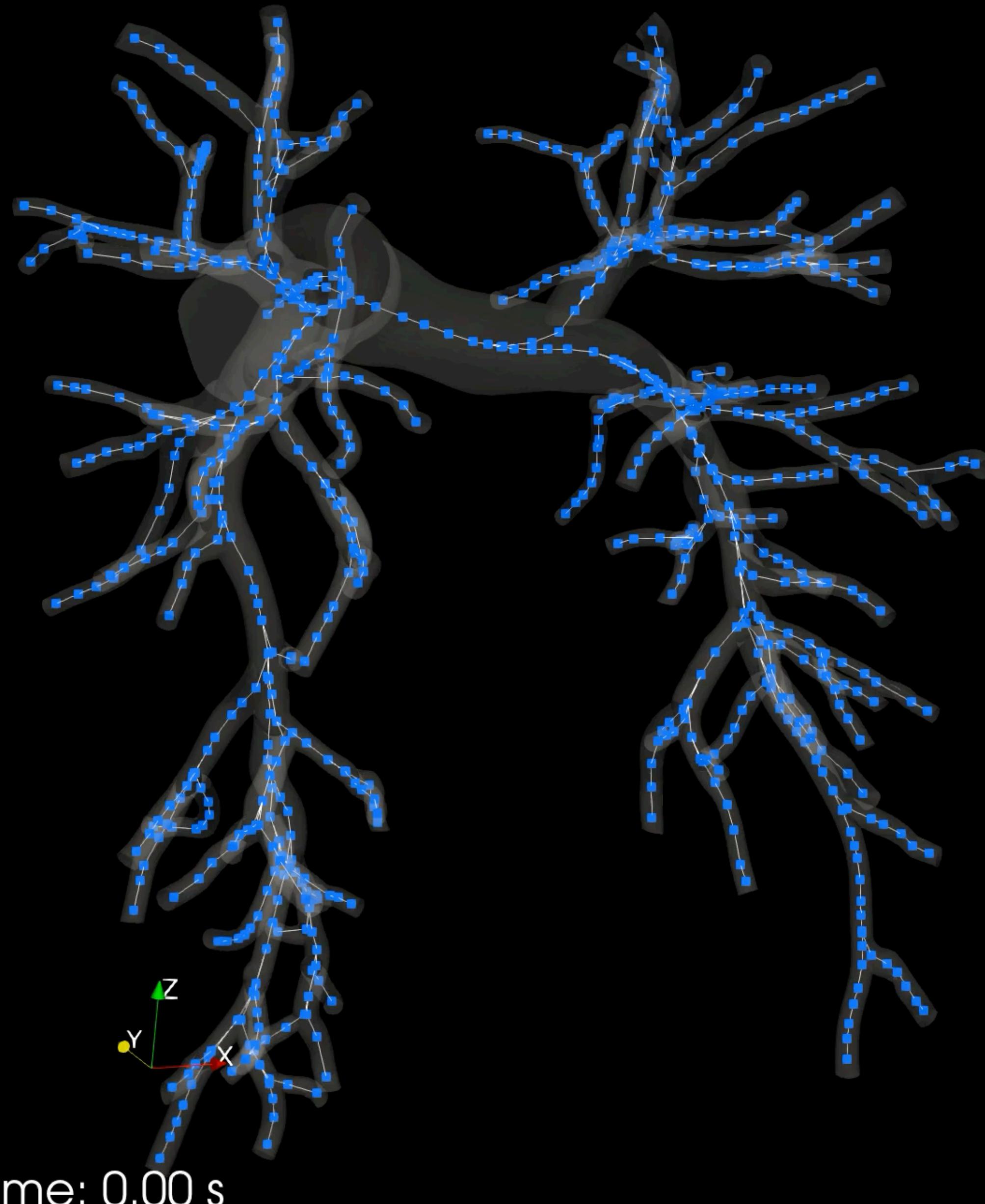


Coarctation

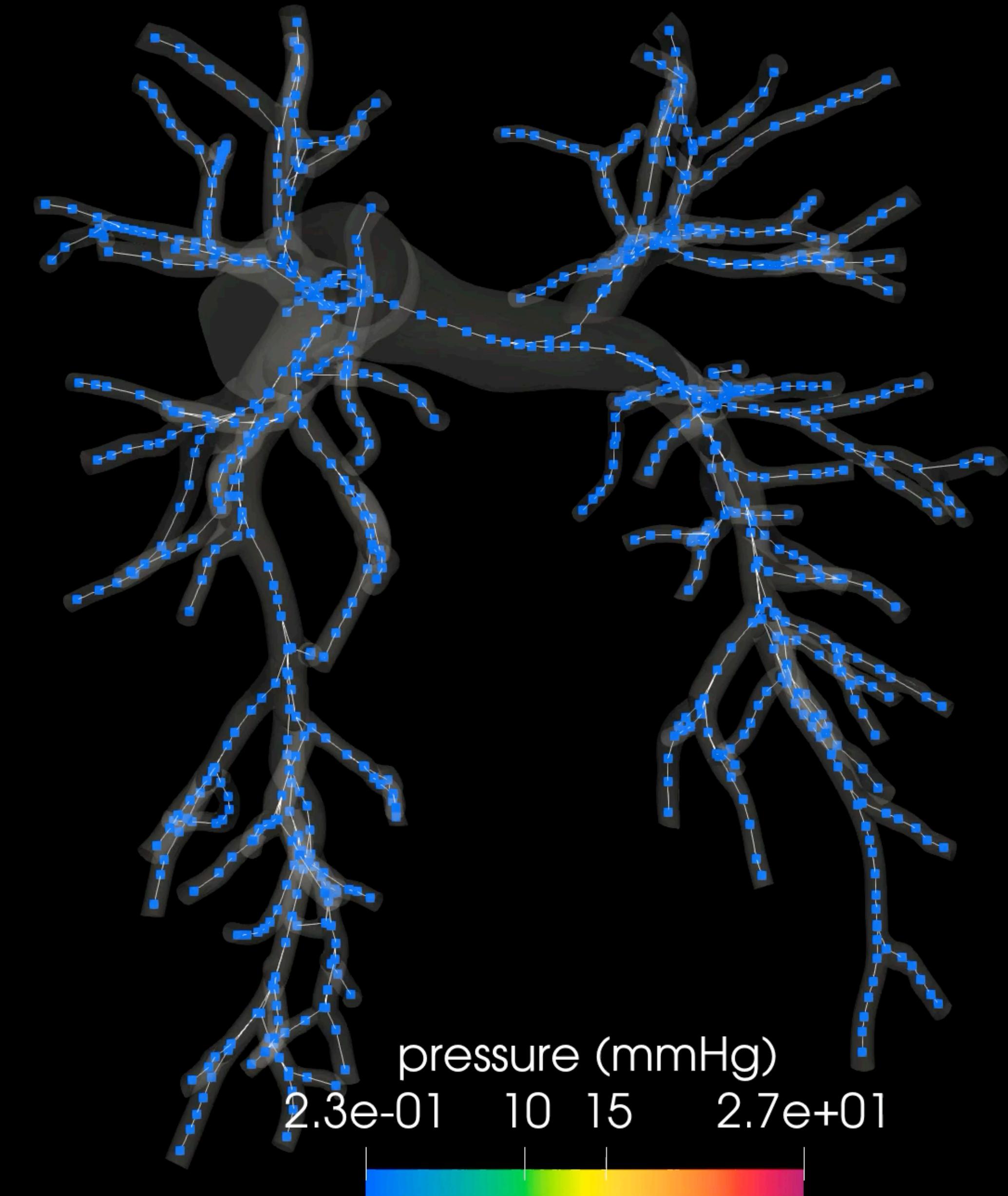
We performed 50 simulations with different boundary conditions for each of these geometries.

3D vs GNN

Ground Truth



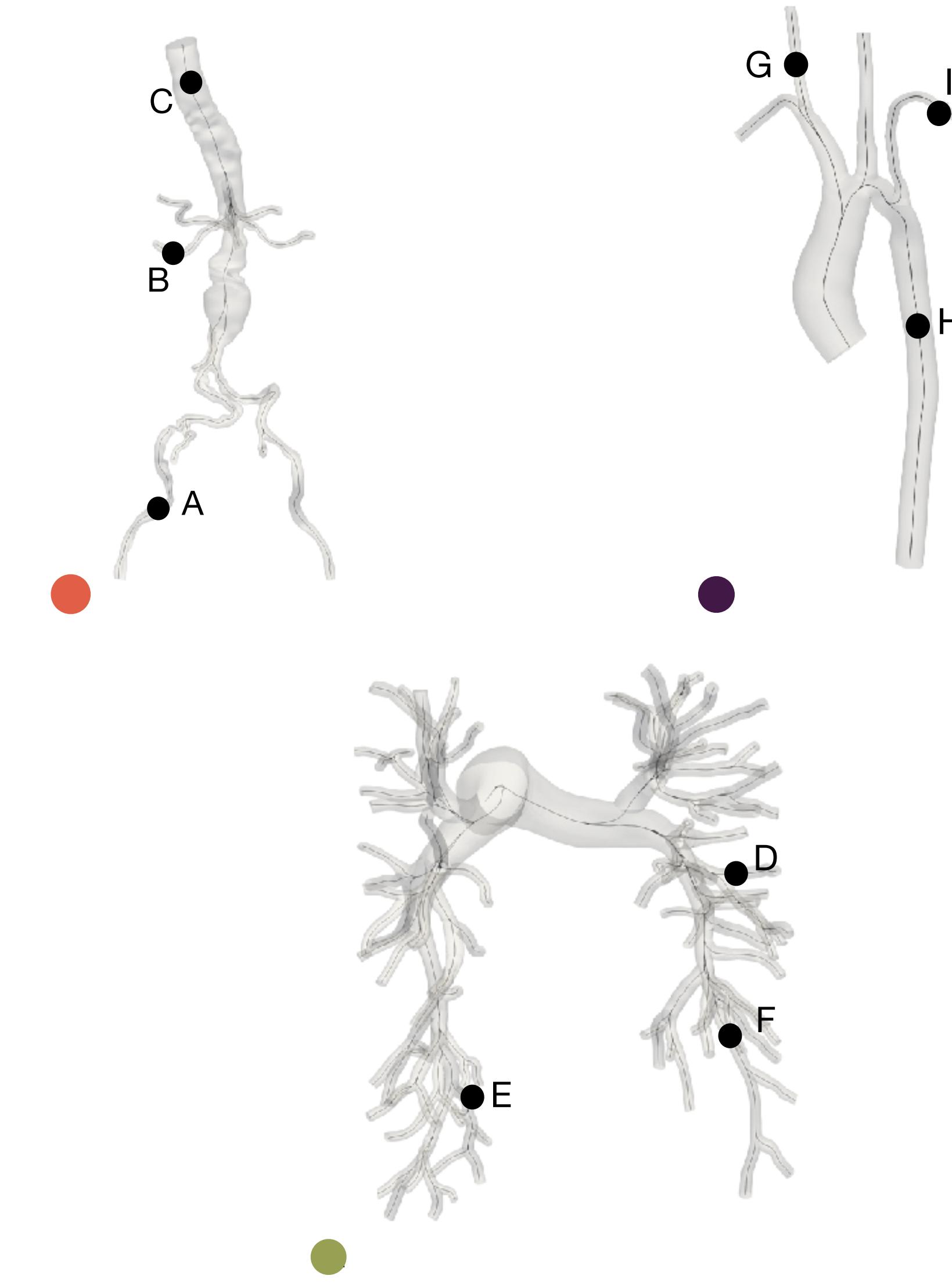
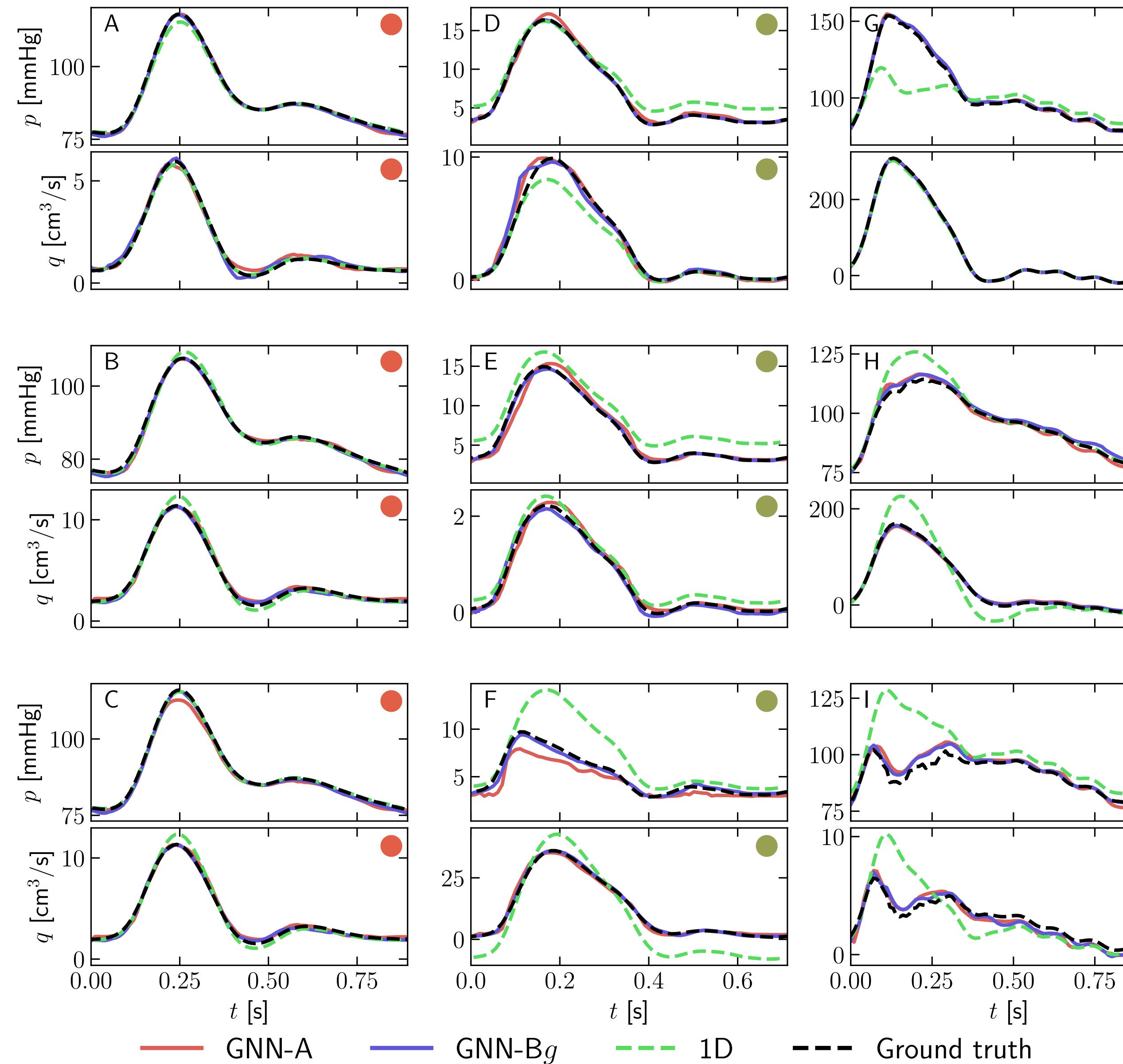
GNN



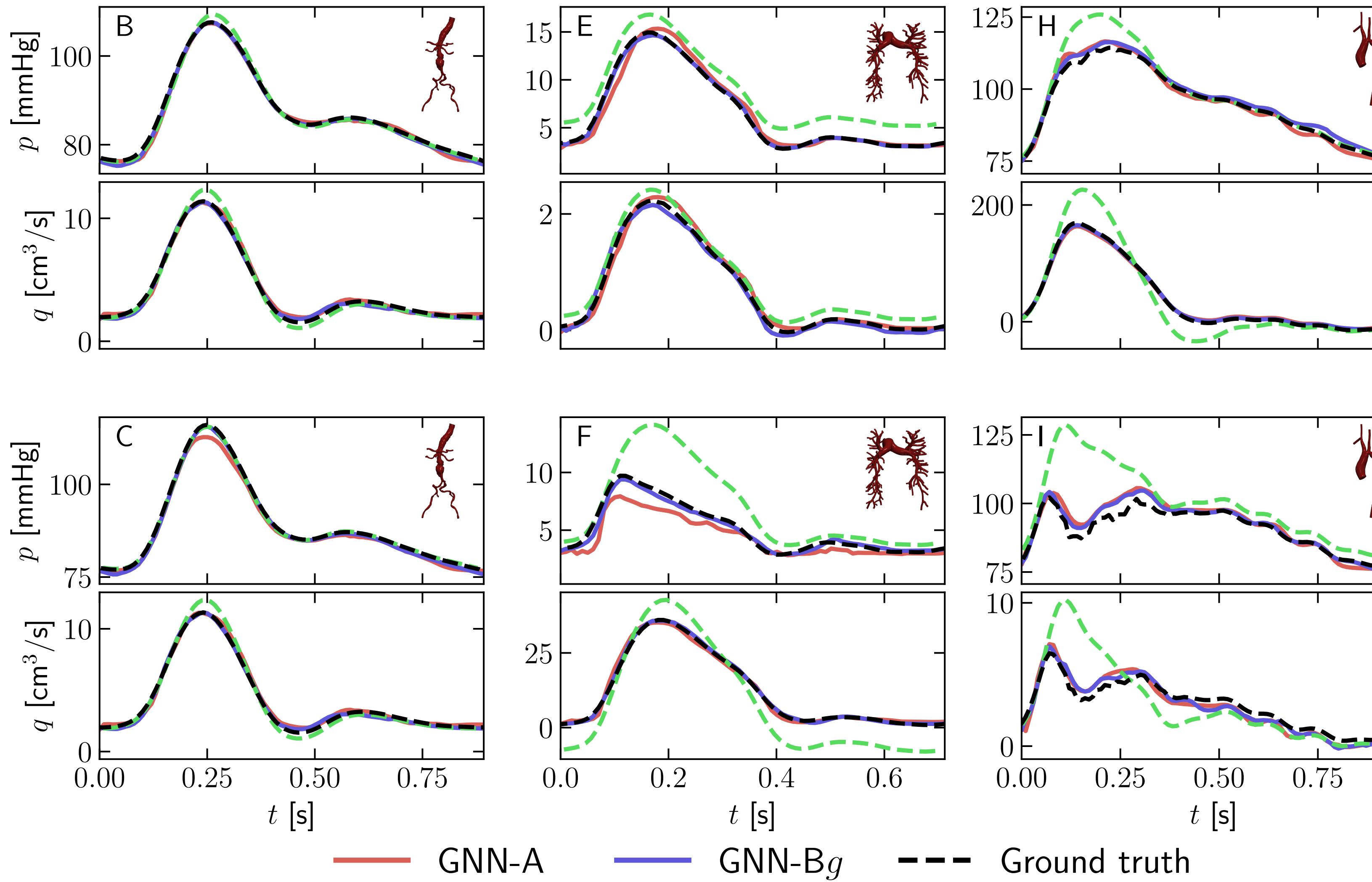
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Qualitative results

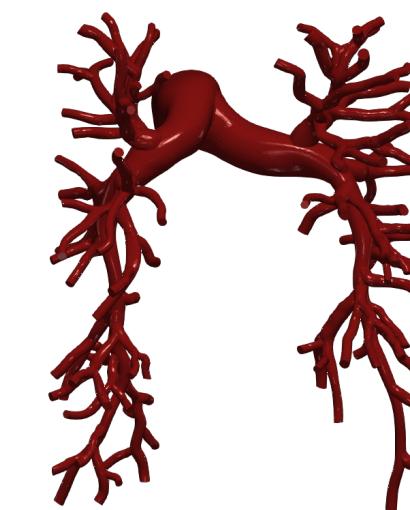
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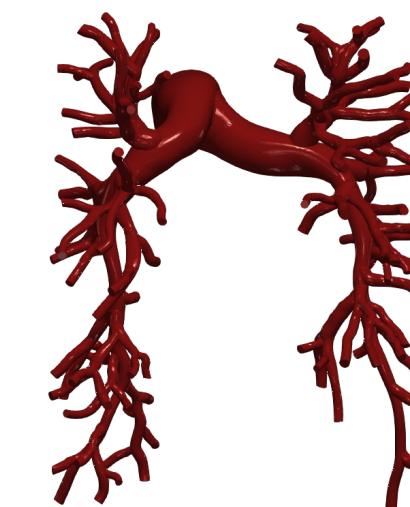
Goal 1: train a single GNN on diverse anatomies.



GNN-A: trained on



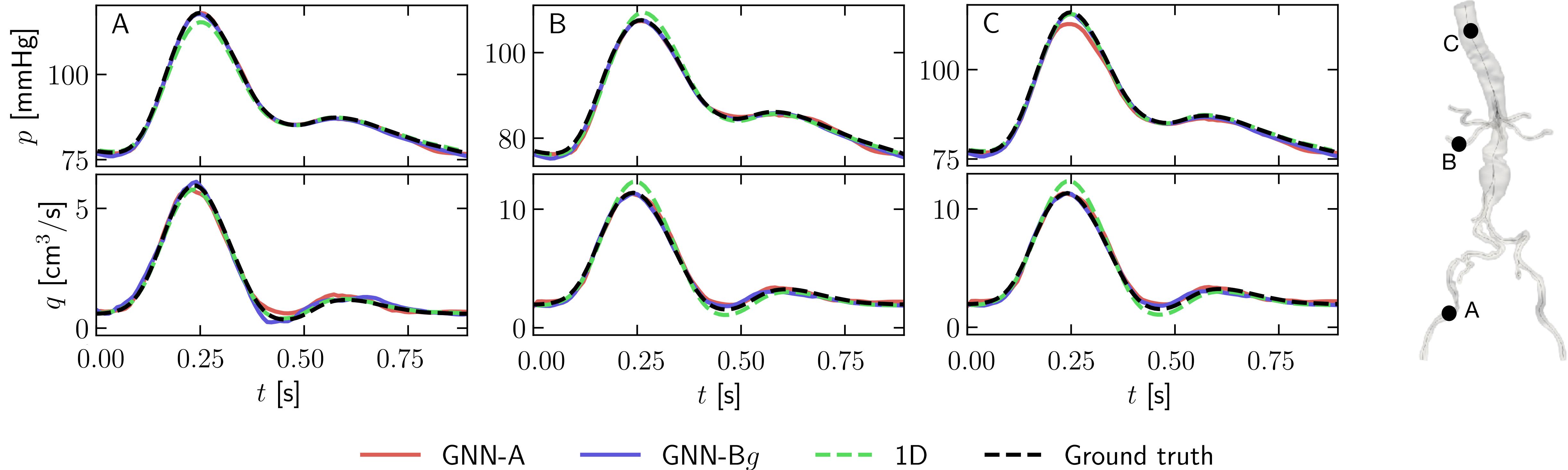
GNN-B_g: trained on



or

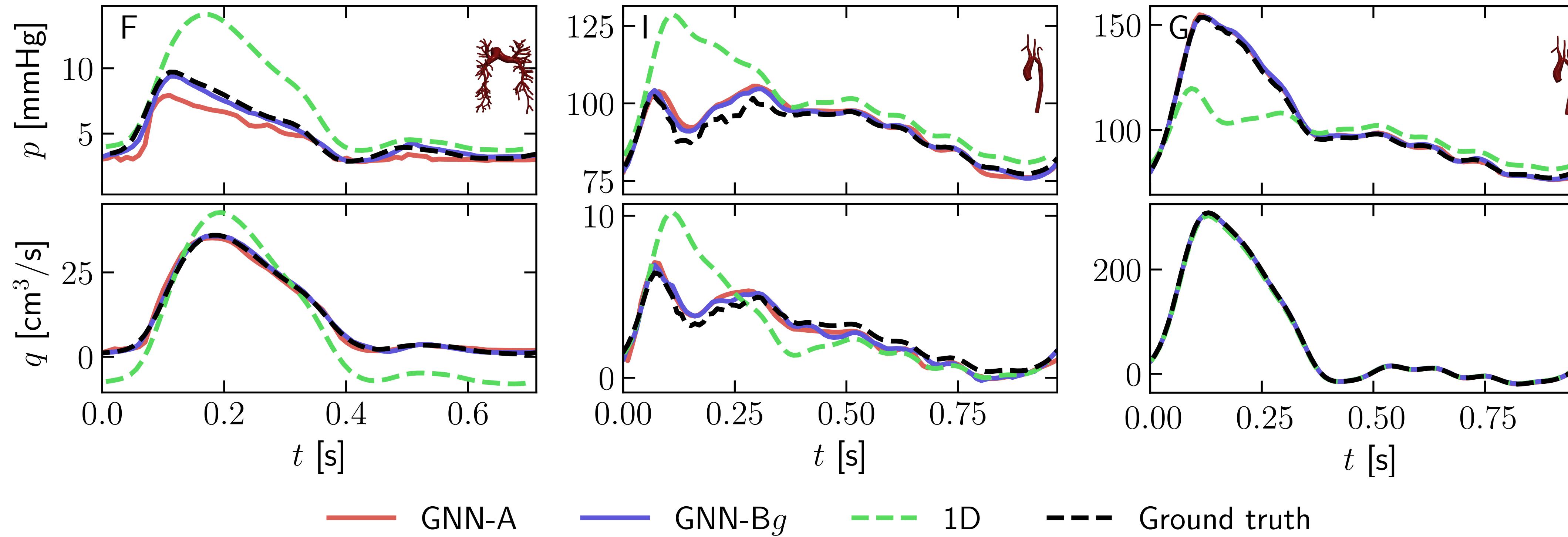


Goal 2: compare performance against physics-based one-dimensional models.

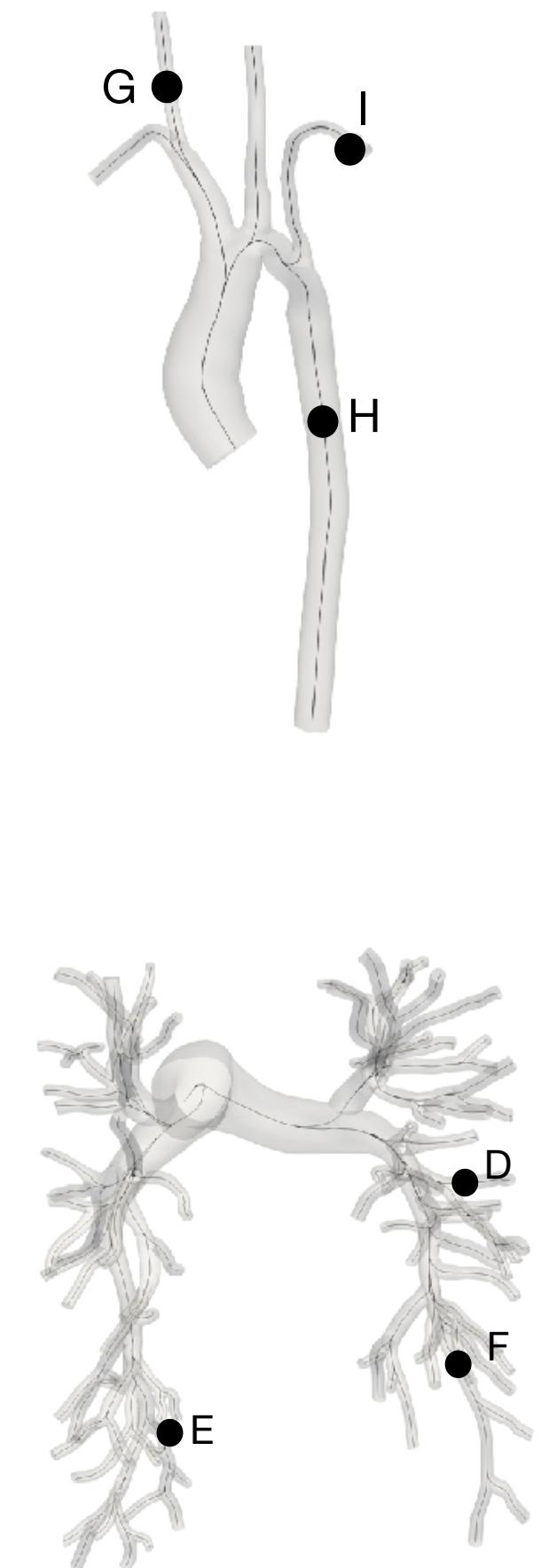


Good agreement on **aneurysm** model

Goal 2: compare performance against physics-based one-dimensional models.



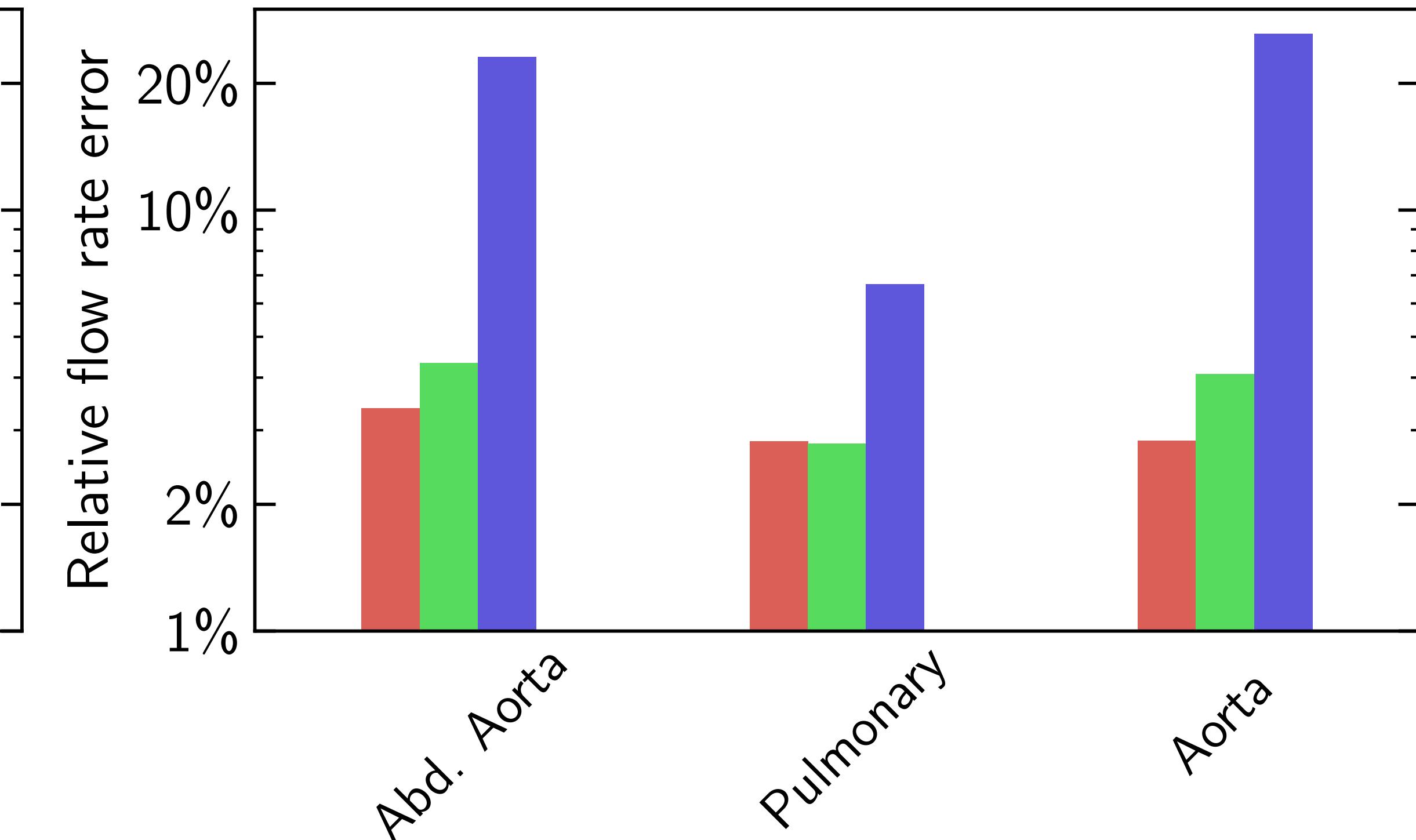
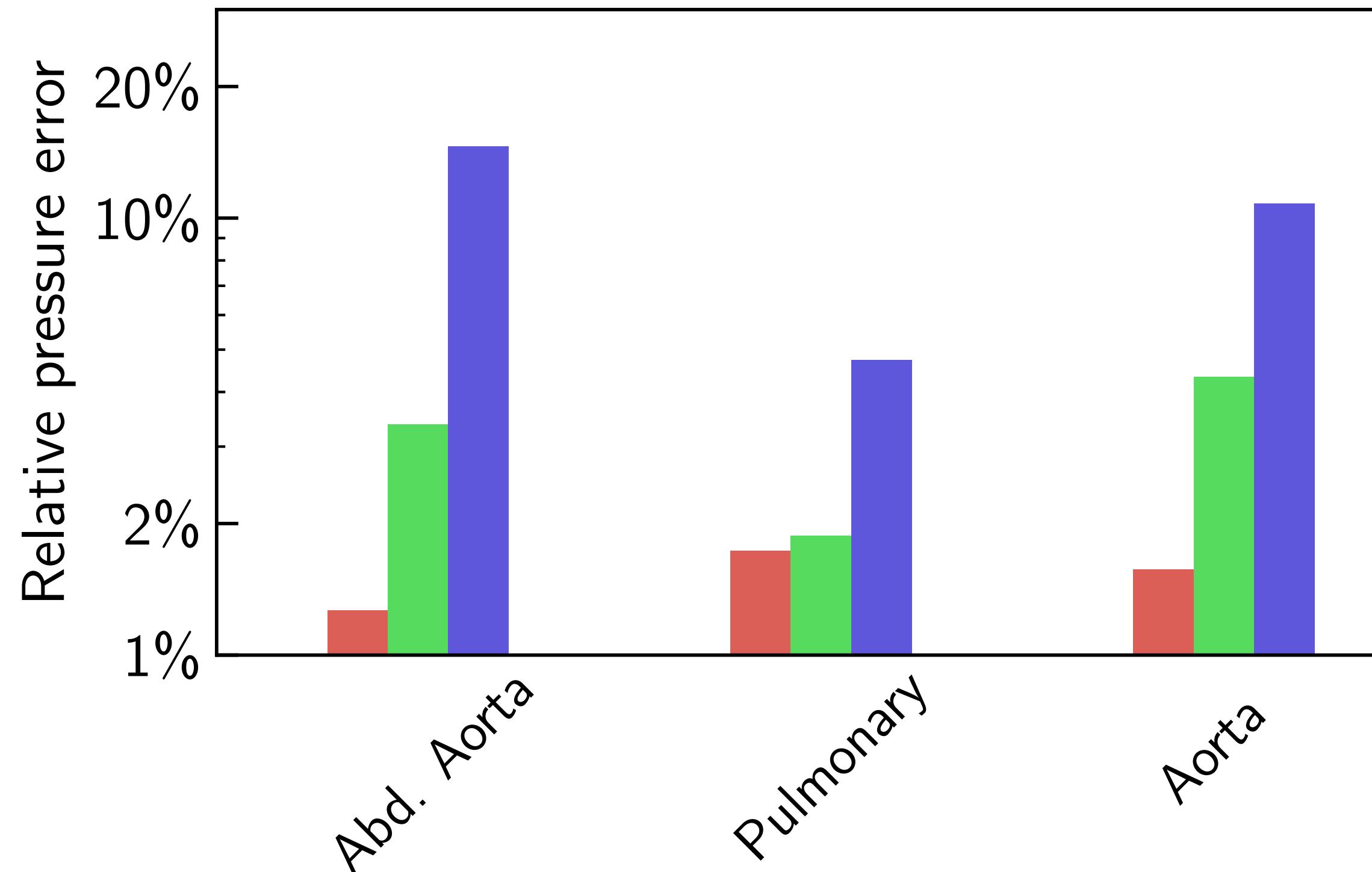
GNN superior on **pulmonary** and **coarctation** models



Ablation study

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GNN-A GNN-A w/o τ GNN-A w/o boundary edges



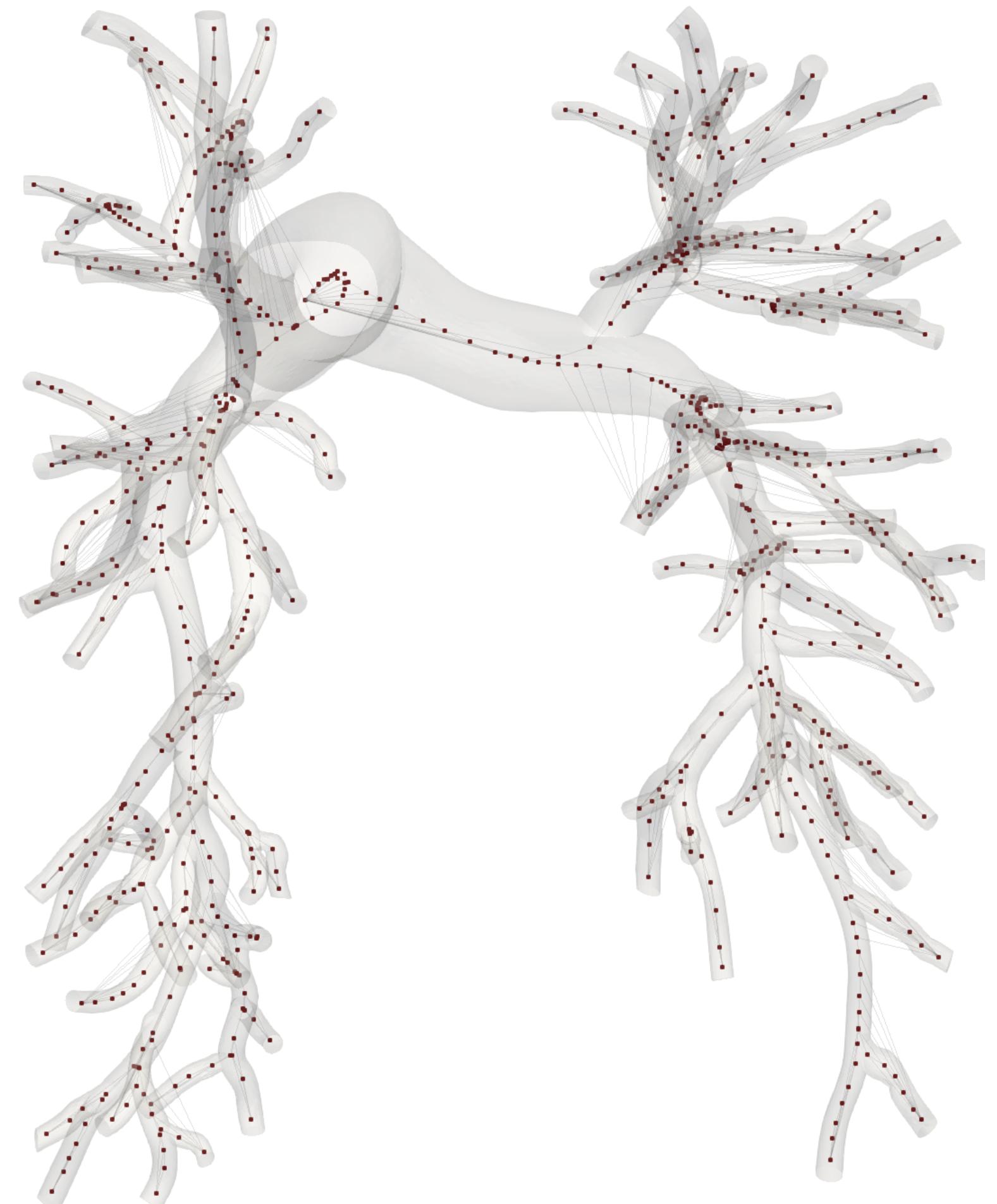
τ : application-specific features

Conclusions

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Graph Neural Networks can be used as **surrogate 1D models.**

They perform better than 1D models **when trained on sufficient data.**



arXiv paper



GitHub repository



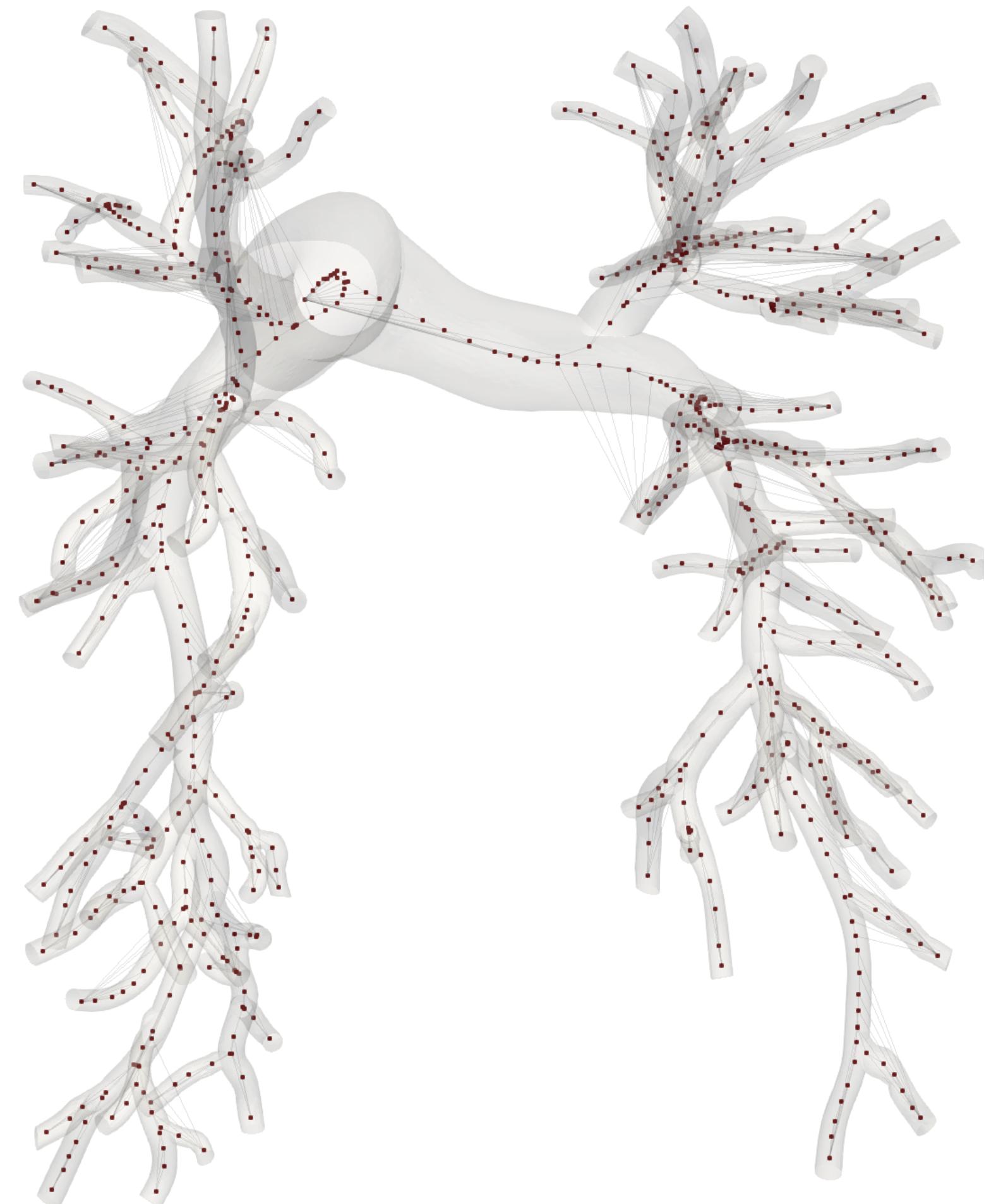
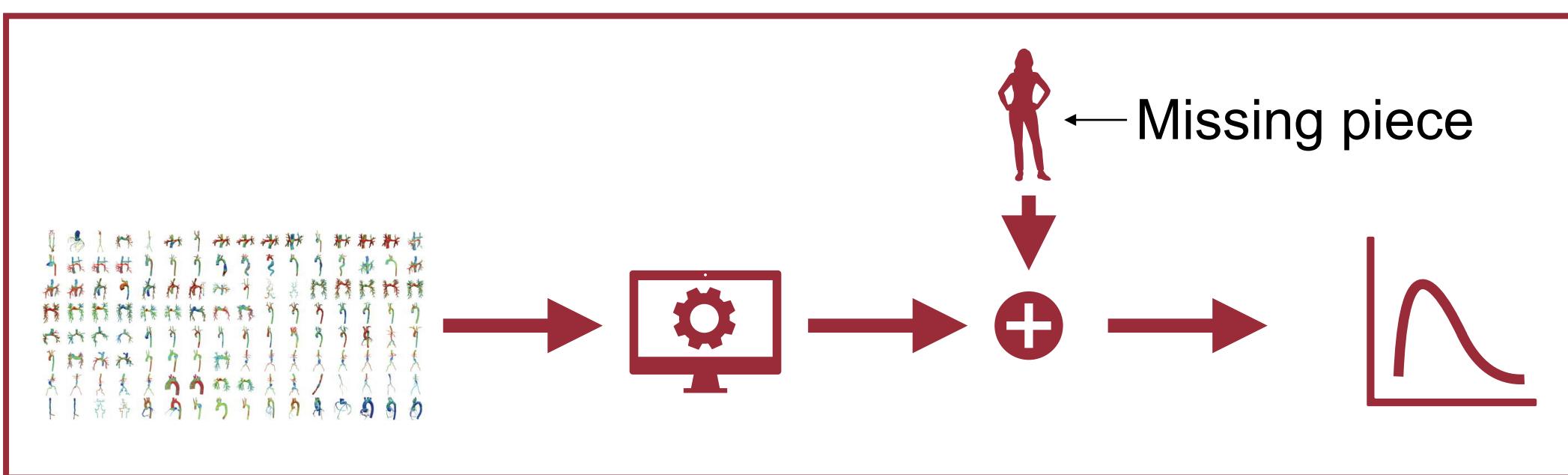
Conclusions

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Graph Neural Networks can be used as **surrogate 1D models**.

They perform better than 1D models **when trained on sufficient data**.

Not there yet, but on the right track



arXiv paper



GitHub repository

